

1 **DEVELOPMENT OF A SIMPLE, LOW COST CHRONOAMPEROMETRIC ASSAY FOR**
2 **FRUCTOSE BASED ON A COMMERCIAL GRAPHITE-NANOPARTICLE MODIFIED**
3 **SCREEN-PRINTED CARBON ELECTRODE.**

4 Phil Nicholas¹, Robin Pittson¹ and John P Hart^{2*}

5 ¹The Gwent Group, Monmouth House, Mamhilad Park, Pontypool, NP4 0HZ, United Kingdom. +44-1495-750505.

6 philip@gwent.org

7 ² Centre for Research in Biosciences, Faculty of Health and Applied Sciences, University of the West of England,

8 Bristol, Coldharbour Lane, Bristol BS16 1QY, UK

9 * Correspondence: john.hart@uwe.ac.uk. Tel.: +44-11-7328-2469

10 **ABSTRACT**

11 This paper describes the development of a simple, low cost chronoamperometric assay, for the measurement of
12 fructose, using a graphite-nanoparticle modified screen-printed electrode (SPCE-G-COOH). Cyclic voltammetry
13 showed that the response of the SPCE-G-COOH enhanced the sensitivity and precision, towards the enzymatically
14 generated ferrocyanide species, over a plain SPCE; therefore the former was employed in subsequent studies.

15 Calibration studies were carried out using chronoamperometry with a 40 µl mixture containing fructose, mediator
16 and FDH, deposited onto the SPCE-G-COOH. The response was linear from 0.1 mM to 1.0 mM. A commercial
17 fruit juice sample was analysed using the developed assay and the fructose concentration was calculated to be 477
18 mM with a precision of 3.03 % (n=5). Following fortification (477 mM fructose) the mean recovery was found to be
19 97.12 % with a coefficient of variation of 6.42 % (n=5); consequently, the method holds promise for the analysis of
20 commercial fruit juices.

21

22 Keywords: Fructose, fructose dehydrogenase, chronoamperometric, screen-printed, graphite, nanoparticles

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26 **1. INTRODUCTION**

27 The ability to precisely and accurately measure the sugar known as fructose has become of considerable interest, to
28 many food companies. For example, the wine manufacturing industry use the concentration of fructose (along with
29 glucose) to predict the alcohol content following fermentation (Guillaume, Delobel, Sablayrolles and Blondin, 2007;
30 Bauer and Pretorius, 2000). The fructose concentration in commercial fruit juices is also an important indicator of
31 the freshness of the food product (Fadel, 2008).

32 Currently, few reports describe the development of amperometric assays for the measurement of fructose, compared
33 with other sugars such as glucose and sucrose (Biscay, Rama, Garcia, Reviejo, Carrazón and García, 2012;
34 Tsujimura, Nishina, Kamitaka and Kano, 2009; Antiochia and Gorton, 2014). One of the current methods, of
35 determining fructose and other simple sugars, involves the °Brix test (Cejpek 2012; Kawahigashi, Kasuga,
36 Okuizumi and Hiradate, 2013), which is based on refractometry; this provides the percentage of total dissolved
37 solids present in the liquid sample. As this method involves refractive index measurements, alcohol can have a
38 detrimental effect on the result, owing to the difference in refractive index between alcohol and water (Dongarea,
39 Buchadeb and Shaligramca, 2015). An alternative approach is based on fourier transform infrared spectroscopy
40 (Reru, Wibowo and Rondonuwu, 2016; Wang, et al., 2010), however this technique is not readily applicable to
41 remote analysis and has a relatively high cost.

42 An attractive alternative approach, which we decided to explore, involves the development of a simple
43 chronoamperometric assay, based on a screen-printed electrode. This is a low cost method, particularly when carbon
44 materials are used in the fabrication of the electrodes. Screen-printed carbon based sensors have been previously
45 developed by our group for the measurement of a wide variety of analytes, (Hughes, Westmacott, Honeychurch,
46 Crew, Pemberton and Hart, 2016; Hughes, Pemberton, Fielden and Hart,2016). We recently demonstrated the
47 possibility of measuring the sugar galactose, using the enzyme galactose oxidase in conjunction with a screen-
48 printed carbon electrode, modified with the mediator cobalt phthalocyanine (Kanyong, Hughes, Pemberton, Jackson
49 and Hart, 2016; Kanyong, Pemberton, Jackson and Hart, 2013). In another paper, we demonstrated the possibility of
50 developing a biosensor for the measurement of glutamate, in a food sample using the enzyme glutamate
51 dehydrogenase integrated with a screen printed carbon electrode. It was possible to carry out the analysis of

52 commercial OXO cubes, after a very simple dissolution and dilution step (Hughes, Pemberton, Fielden and Hart,
53 2015). Consequently, we decided to explore the possibility of developing a simple electrochemical sensor system,
54 for the measurement of fructose in food samples, based on screen-printed carbon electrodes (SPCEs) in conjunction
55 with fructose dehydrogenase. As the incorporation of nanoparticles in the chronoamperometric measurement of
56 glutamate proved to be advantageous, we decided to investigate a novel nano-material in the present study.

57 This paper describes the optimization of the components and operating conditions, of a chronoamperometric assay
58 for fructose; this incorporated fructose dehydrogenase with a nanoparticle modified screen-printed electrode. The
59 possibility of measuring the sugar, in a commercial fruit juice, will be discussed.

60

61 **2. EXPERIMENTAL**

62 **2.1 Chemical reagents**

63 D-fructose dehydrogenase was obtained from Toyobo Enzymes (Japan). (www.toyobo-global.com)

64 The graphite-nanoparticles (graphite modified with carboxylic acid) in solution (C2131210D1) were obtained from
65 Gwent Electronic Materials. (www.gwent.org).

66 Apple juice was obtained from a local supermarket.

67 All other chemicals and reagents were obtained from Sigma-Aldrich (UK). (www.sigmaaldrich.com)

68 McIlvaine buffer was prepared by mixing 0.2 M citric acid (containing 0.2 M KCl) with 0.4 M disodium phosphate
69 (containing 0.2 M KCl) to produce a final pH of 4.5.

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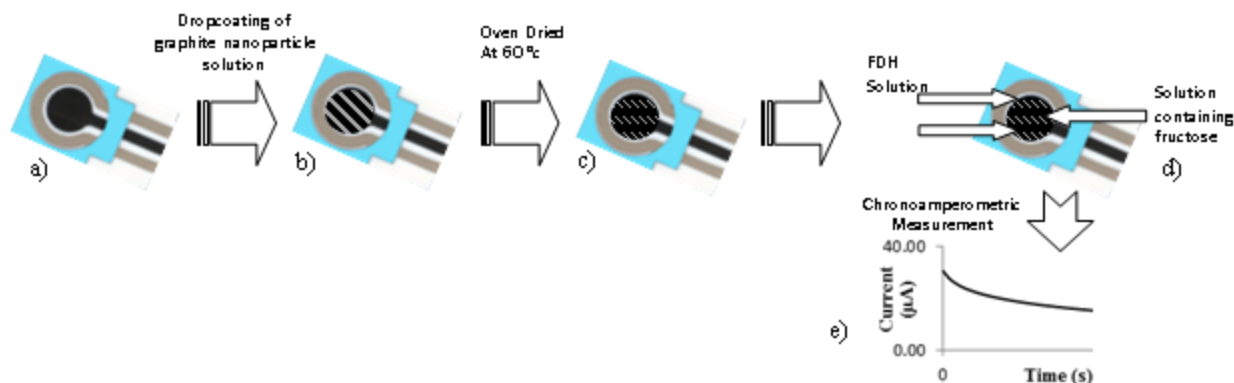
71 **2.2 Apparatus and Instrumentation**

72 All electrochemical measurements were conducted with a two-electrode system, consisting of a screen-printed
73 working electrode (GEM code: C2030519P4), Ag/AgCl reference electrode (GEM Product Code: C61003P7) both
74 screen-printed onto valox (a semi-crystalline material based on polybutylene terephthalate and polyethylene

75 terephthalate polymers; Cadillac Plastics Swindon, UK). The diameter (6 mm) of the working electrode was defined
76 using a dielectric ink (GEM Product Code: D2070423P5) a concentric silver/silver-chloride served as the
77 counter/reference electrode, (GEM Electrode Design: BE2110916D1). For further studies, the surface of the
78 working electrode was modified by addition of 10 μ l of graphite-nanoparticles (1.787 mg ml⁻¹) (GEM code:
79 C2131210D1).

80
81 The working and reference electrodes were connected to the potentiostat with GEM electrode connector (GEM
82 Code: CON002). All electrochemical studies were performed using an AutoLab [μ AutoLab Type II], with General-
83 Purpose Electrochemical Software (The Netherlands). Data were further analyzed with Microsoft Excel.

84 Fig.1 summarises the fabrication and operation of the fructose biosensor



85 *Fig.1. Scheme showing the fabrication of the fructose biosensor and chronoamperometric measurement of fructose:*
86 *a) Plain SPCE; b) SPCE with deposition of nanoparticles in solution; c) SPCE with dried nanoparticles; d) addition*
87 *of 10 μ l FDH, 10 μ l ferricyanide; 20 μ l of solution containing fructose; e) Chronoamperometric measurement*
88

89 It should be noted that during the fabrication of the nano-particle modified electrodes, the deposited nano-particles
90 were confined to the working area by the hydrophilicity of the carbon and the hydrophobicity of the underlying
91 valox substrate. This ensured that the working area remained the same between the unmodified and modified
92 working electrodes and was confirmed by visual inspections.

93 2.3 Procedures

94 Cyclic voltammetry was performed by depositing a 300 μl aliquot of 0.5mM ferriykanide, in 0.1 M phosphate buffer
95 pH 7.5 containing 0.1 M potassium chloride onto the surface of the screen-printed carbon electrodes. Cyclic
96 voltammetry was performed using the following conditions: initial and final potential +0.8 V; switching potential –
97 0.4 V; scan rate 10 mV s^{-1} . Potential held at +0.8 V for 20 seconds before initial cycle.

98 Calibration studies were performed using chronoamperometry with standard solutions of fructose, over the
99 concentration range 0.20 mM to 32.00 mM, in water; FDH was dissolved in McIlvaine buffer to produce
100 concentrations of either 50 U ml^{-1} or 200 U ml^{-1} . The measurement procedure involved the deposition of 20 μl of
101 either enzyme solution, onto the screen printed transducer, followed by 10 μl of 12 mM ferricyanide and 10 μl
102 fructose standard. Following an incubation time of 180 s (open circuit), with initial 20 s of agitation, the potential
103 was stepped from open circuit to +0.3 V vs Ag/AgCl. Currents were measured 20 s after application of the voltage
104 and these values were used to plot calibration graphs.

105

106 **2.4 Analytical Application**

107 A preliminary study was performed with the commercial apple juice, to deduce an appropriate dilution procedure. A
108 series of dilute apple juice solutions were prepared by mixing the neat sample with deionized water to produce final
109 dilutions in the range of 1/2 and 1/512, of the original concentration. The analysis was carried out using
110 chronoamperometry as described above, and from the results the optimum dilution that produced a signal within the
111 linear range was deduced.

112 The method of standard addition was performed with the optimum dilution of the apple juice (with deionized water).
113 This was achieved by mixing the diluted apple juice with different concentration fructose standards, so that the final
114 concentration of the standard added was between 0.1 and 0.8 mM. This procedure was repeated 5 times, with each
115 data point being replicated 5 times. The concentration of fructose in the original sample was obtained from this data,
116 together with the precision of the measurements.

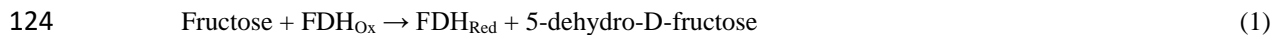
117 The recovery of added fructose was ascertained by spiking the original sample with 477.2 mM of fructose (this was
118 equal to the concentration found in the undiluted sample). The same chronoamperometric procedure was used, as
119 previously described.

120

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122 3. RESULTS AND DISCUSSION

123 3.1 Principles of the Amperometric Measurement of Fructose



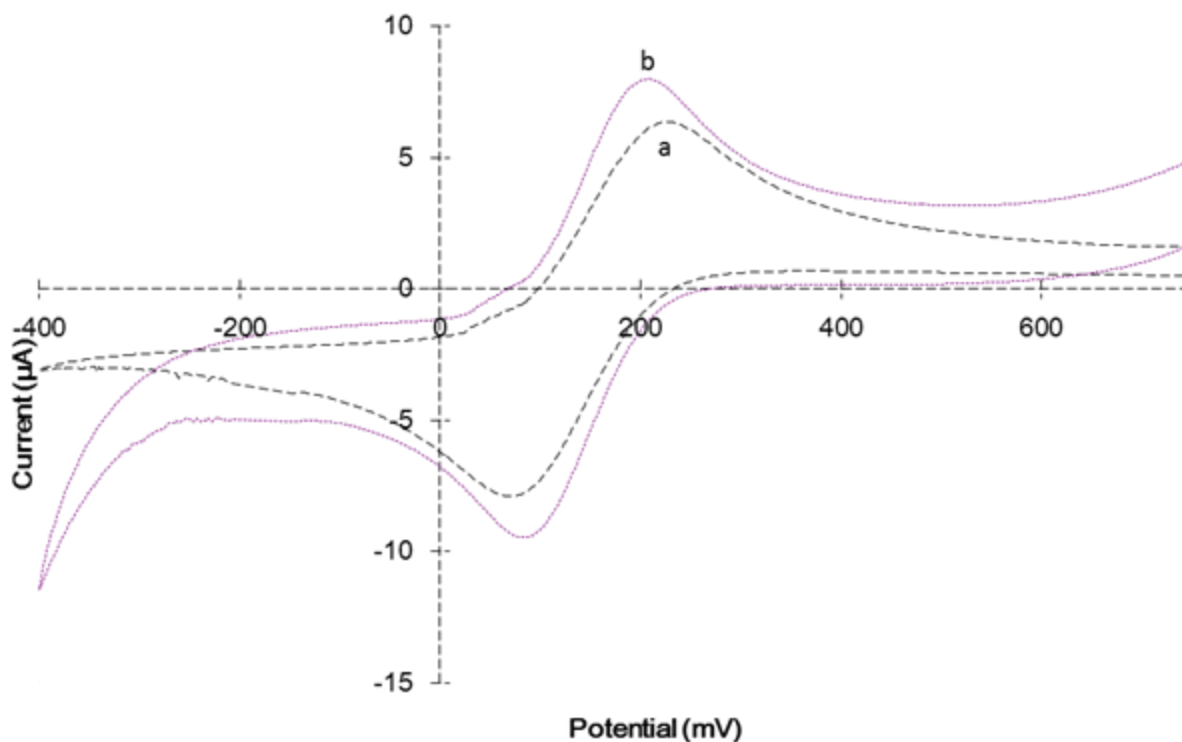
127 Equations (1)-(3) summarise the sequence of reactions involved in the chronoamperometric measurement of
128 fructose, at the surface of a SPCE-G-COOH. Initially, D-fructose dehydrogenase (FDH_{Ox}) is reduced by fructose
129 (eqn1) and this reduced form of the enzyme (FDH_{Red}) reduces ferricyanide (Fe^{3+}) to ferrocyanide (Fe^{2+}) (eqn2); the
130 oxidized form of the enzyme (FDH_{Ox}) is regenerated during the latter reaction. At a potential of +300 mV,
131 ferrocyanide is oxidised back to ferricyanide (eqn3), resulting in the analytical response. Prior to the application of
132 the applied potential, an incubation time of 3 minutes is allowed for the enzymatic oxidation of fructose; the reaction
133 involving ferricyanide results in the conversion of two molecules of the mediator for every molecule of fructose.
134 The magnitude of the resulting electrocatalytic current is proportional to the concentration of fructose, over the
135 range of interest.

136

137 3.2 Cyclic Voltammetric Behaviour

138 An initial study was performed in order to investigate the effect of modifying the SPCE surface with COOH-
139 graphite nanoparticles. The nanoparticles were drop coated onto the plain screen printed electrode (and dried) and
140 interrogated by cyclic voltammetry, using a solution of 0.5mM ferricyanide, in 0.1 M phosphate buffer pH 7.5
141 containing 0.1 M potassium chloride.

142 Fig.2 shows a comparison of the cyclic voltammetric behaviour of an unmodified screen printed carbon electrode (a)
143 and a SPCE with 17.89 μg deposited onto the surface (b). The increase in current magnitude may be explained by an
144 enhancement in the electron transfer properties, from ferrocyanide to the modified electrode surface. It should be
145 mentioned that the coefficient of variation was determined for the anodic peak currents; this was found to be
146 reduced from 6.73% to 4.75% ($n=9$), for plain SPCE and SPCE-G-COOH, respectively. For the development of the
147 chronoamperometric assay this improved precision, together with the improved sensitivity, can be considered of
148 importance to the development of a reliable analytical procedure.



149
150 *Fig.2. A typical cyclic voltammograms obtained with 0.5 mM ferricyanide in 0.1 M phosphate buffer pH 7.5*
151 *containing 0.1 M potassium chloride using a scan rate of 10 mV s⁻¹: for (A) plain SPCE (B) SPCE-G-COOH.*
152 *Voltammetric conditions: starting potential +0.8 V, switching potential -0.4 V.*

153
154 Fig.2 also shows that there is a difference in the peak separation (ΔE_p) for the two voltammetric scans, for the plain
155 SPCE and SPCE-G-COOH; these values were 169 mV and 148 mV, respectively. Both values indicate that the

156 redox reaction is quasi-reversible; however, the reaction at the SPCE-G-COOH appears to be more favourable.
157 Further evidence for this is obtained the charged transfer coefficient (α), using equation 4 (Kirsch, Hart, Bird,
158 Luxton and McCalley, 2001) where is n is the number of electrons involved in the rate determining step.

159
$$\alpha n = \frac{0.048}{E_p(V) - E_p(V)} \quad (4)$$

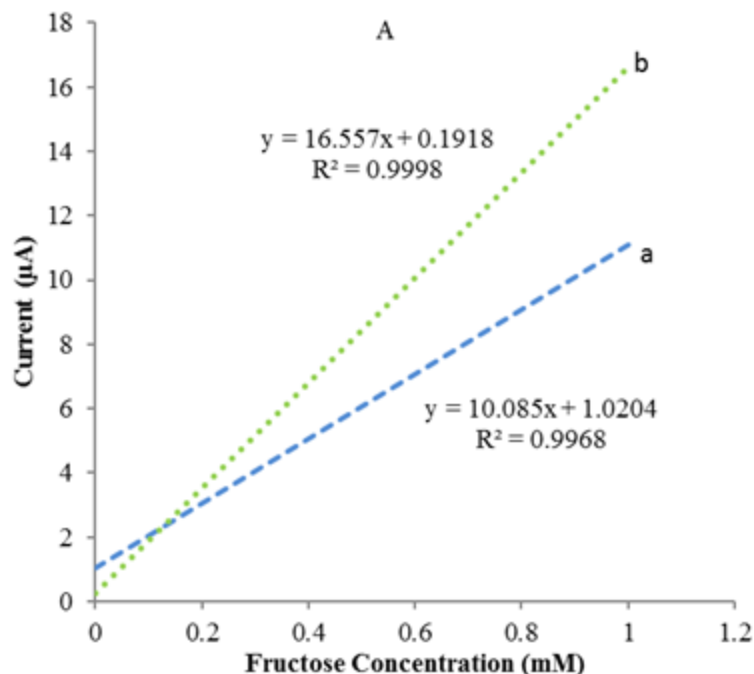
160 The α values (obtained using n=1) for the plain SPCE and SPCE-G-COOH were calculated to be 0.56 and 0.64,
161 respectively. Therefore the electron transfer kinetics are more favourable in the case of the SPCE-G-COOH, which
162 indicates that this sensor has superior electrochemical characteristics, which should lead to more reproducible
163 measurements. It should be mentioned that both of these values are better that reported for a commercial graphite
164 electrode (reported $\alpha = 0.486$) (Botasini, Marti and Méndez, 2016). From these results, it appears that the reason for
165 the increase in current magnitude occurs as a result of improved electron transfer, rather than a simple increase in
166 electrode surface. Consequently, all further studies were performed using the SPCE-G-COOH electrodes.

167 **3.3 Calibration Studies, using chronoamperometry with a SPCE-G-COOH**

168 We began this study by investigating the SPCE-G-COOH modified with 1 U of FDH deposited onto the surface; a 3
169 minute incubation time was employed at room temperature, at open circuit. A calibration study was carried out over
170 the range 0.10 to 1.00 mM fructose; a linear response was obtained under these conditions and the slope was found
171 to be 10.085 $\mu\text{A mM}^{-1}$, Fig.3A(a).

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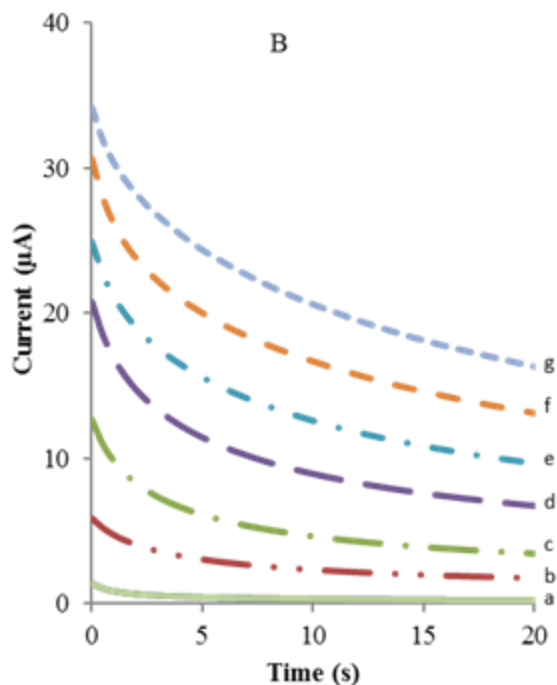
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175 Fig. 3A Calibration plots obtained for fructose using a) 1 unit of FDH with a 3 minute incubation time; b) 4 units of
 176 FDH with a 3 minute incubation time.

177 In order to investigate the possibility of increasing the sensitivity of the chronoamperometric assay, the enzyme
 178 loading was increased to 4 units, on the sensor surface. Fig.3A(b) shows the resulting calibration plot, obtained
 179 under these conditions and demonstrates a linear range of up to 1 mM, with a slope of $16.6 \mu\text{A mM}^{-1} \pm 0.4 \mu\text{A mM}^{-1}$.
 180 Fig.3B shows typical chronoamperograms obtained for standard solutions of fructose, over the range 0.10 mM to 1.00
 181 mM; currents were measured at 20 seconds after the potential was initiated. It should be mentioned that the
 182 sensitivity achieved with the COOH-G-SPCE was found to be higher than that reported in several papers. The
 183 following sensitivity values have been normalised from the original papers to give sensitivity $\mu\text{A mM}^{-1} \text{cm}^{-2}$, which
 184 allows comparison with the current assay: Nicholas, et al. 2017 (current study) $58.56 \mu\text{A mM}^{-1} \text{cm}^{-2}$; Biscay, Rama,
 185 García, Reviejo, Carrazón, García, 2012 (ferrocyanide modified SPCE) $9.95 \mu\text{A mM}^{-1} \text{cm}^{-2}$; Trivedi, et al. 2009
 186 (amperometric biosensor using FDH) $2.19 \mu\text{A mM}^{-1} \text{cm}^{-2}$; Antiochia, et al., 2014 (osmium-polymer mediated
 187 biosensor) $1.95 \mu\text{A mM}^{-1} \text{cm}^{-2}$. At this point it was considered that the optimised chronoamperometric assay
 188 conditions would be suitable for the analysis of a range of fruit juices; however for evaluation purposes a typical
 189 commercial apple juice was selected. This is described in the following section.



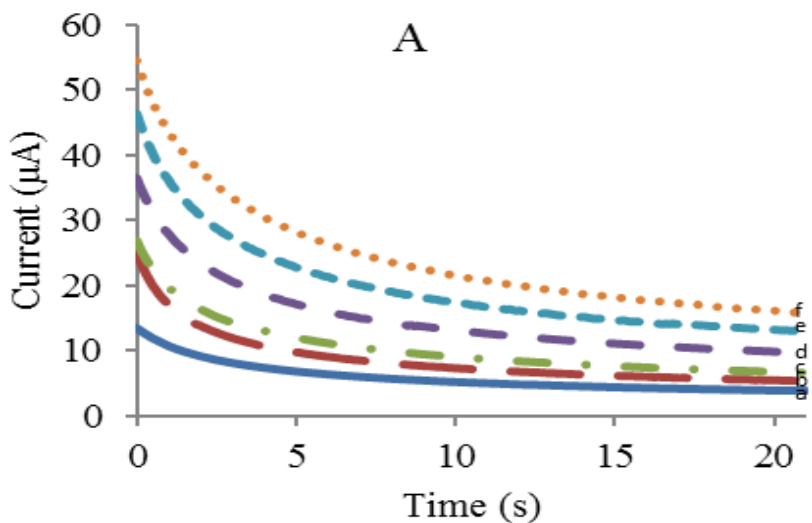
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191 *Fig. 3B C* chronoamperograms obtained with the fructose sensor for various concentrations of fructose: a) 0.00 mM;
 192 b) 0.10 mM; c) 0.20 mM; d) 0.40 mM; e) 0.60 mM; f) 0.80 mM; g) 1.00 mM. Sensor operation performed with 4 units of
 193 FDH with a 3 minute incubation time.

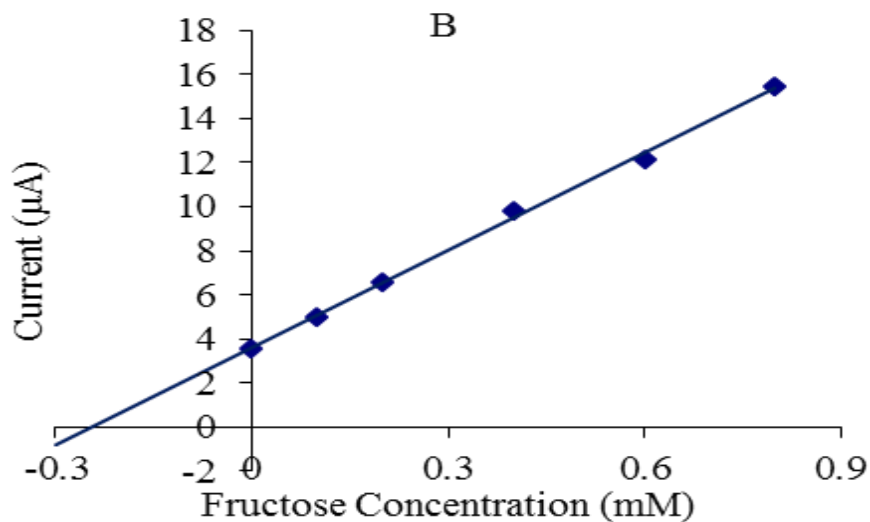
194

195 3.4 Analytical Application

196 In order to evaluate the chronoamperometric assay for the measurement of fructose in commercial fruit juices, a
 197 typical apple juice product (obtained from a local supermarket) was analysed using the developed assay. Fig.4A
 198 shows typical chronoamperometric responses obtained for the samples of apple juice, diluted 500 times (with
 199 deionised water (4A a) and after the addition of standard fructose solutions (4A b-f). Fig.4B shows a typical
 200 standard addition plot, from which the original concentration of fructose was determined.



201
 202 Fig.4A. Typical chronoamperograms obtained with SPCE-G-COOHs for different concentrations of D-fructose:
 203 a)Apple Juice(AJ), b)0.10 mM, c)0.20 mM, d)0.40 mM, e)0.60 mM and f)0.80 mM. Incubation time at open circuit
 204 was 180 s, followed by applied potential of + 0.3 V vs Ag/AgCl. The supporting electrolyte was 0.1 M phosphate
 205 buffer containing 0.1 M potassium chloride.



207
 208 Fig.4B. Typical standard addition plot, obtained using chronoamperometric currents measured 20 s after
 209 application of +0.3 V vs Ag/AgCl

210

211 Table 1 shows a summary of the data obtained for the original fructose concentration of the unspiked apple juice. It
212 should be noted that column 2 refers to the concentration on the screen-printed transducer; column 3 refers to the
213 concentration of fructose corrected for the dilution factors.

214 **Table 1. Concentration of fructose determined in dilute fruit juice and calculated original values (n=5).**

| Sample | Concentration determined after dilution (mM) | Calculated Original Fructose Concentration (mM) |
|---------------------------|---|--|
| 1 | 0.245 | 490.0 |
| 2 | 0.235 | 470.0 |
| 3 | 0.240 | 480.0 |
| 4 | 0.245 | 490.0 |
| 5 | 0.228 | 456.0 |
| Mean | 0.239 | 477.2 |
| Standard Deviation | 0.007 | 14.46 |
| CV% | 3.031 | 3.031 |

215

216 The data in the Table 1 indicates that the mean original concentration of fructose was 477.2 mM; the precision data
217 of 3.031 % suggests that the method shows promise for analysis for fructose in fruit juices.

218 It is known that ascorbic acid is present in apple juice of concentrations around 2.15 mM (SELFNutrition Data,
219 2014). In order to determine whether this vitamin would affect the response obtained for fructose, in the apple juice
220 sample, a fixed concentration of 2.15 mM ascorbate was added to the neat apple juice followed by dilution (as
221 described earlier). The resulting chronoamperograms did not show any increase in anodic current for any of the
222 solutions shown in Table 1. This is perhaps not surprising bearing in mind the high ratio of fructose to ascorbic acid,
223 present in the sample. This study demonstrated that ascorbic acid at the levels present in the commercial apple juice
224 did not influence the magnitude of the fructose response; therefore no complicated sample preparation procedures
225 were required. The recovery of fructose, added to the original apple juice sample is summarised in Table 2.

226 **Table 2. Recovery of added fructose to original fruit juice sample (n=5).**

| Sample | Original Concentration (mM) | Concentration Added (mM) | Concentration Found (mM) | Fructose Recovered (mM) |
|--------|-----------------------------|--------------------------|---------------------------|-------------------------|
| 1 | 477.2 | 477.2 | 951.88 | 474.68 |
| 2 | 477.2 | 477.2 | 934.28 | 457.08 |
| 3 | 477.2 | 477.2 | 1010.08 | 532.88 |
| 4 | 477.2 | 477.2 | 953.79 | 476.59 |
| 5 | 477.2 | 477.2 | 992.68 | 515.48 |
| | | | Average | 491.34 |
| | | | Standard Deviation | 31.53 |
| | | | CV% | 6.42 |
| | | | Mean Recovery | 97.12 % |

227

228 The data in Table 2 shows that the mean recovery of added fructose is 97.12 % and the co-efficient of variation of

229 6.42 %. Clearly the data shown in Table 1 and Table 2 demonstrates that the chronoamperometric bioassay should

230 give reliable data for the analysis of fructose concentration in fruit juice products.

231

232 **4. Conclusion**

233 This paper describes the development of a simple, low cost chronoamperometric assay, based on the electrocatalytic

234 oxidation of FDH with a SPCE-G-COOH, and its evaluation using a commercial fruit juice. It was shown that the

235 incorporation of modified graphite nanoparticles enhanced the sensitivity and improved the precision of the response

236 towards the enzymatically generated ferrocyanide species, compared with a plain SPCE. The calibration studies

237 indicated that a linear response could be obtained up to 1.00 mM fructose using a mediator concentration of 3 mM.

238 Consequently, the proposed biosensor could be adapted for a wide range of food products. It should be mentioned

239 that sample preparation only involves the dilution of the sample prior to analysis; which is performed only on 40 µl,

240 of solution, applied directly onto the sensor surface. Therefore, it is readily feasible that this approach could be
241 performed near to the point of production and used as a quality control method. It should be mentioned that the
242 detection limit of 8 μM was achieved in the current study; however the detection limits in the commonly used Brix
243 test has a limit of detection of 556 μM (Cejpek 2012) and a method involving HPLC with UV-visible spectrometry
244 had reported a detection limit of 222 μM (Bever HAJM, Wijntje R and de Haan AB 2005). Therefore, we believe
245 that the current amperometric fructose bioassay, employing a SPCE-G-COOH, holds promise for applications where
246 other conventional techniques do not have the desired detection limit.

247

248 This research did not receive any specific grant from funding agencies in the public, commercial, or
249 not-for-profit sectors.

250

251

252 **Captions**

253 *Fig.1. Scheme showing the fabrication of the fructose biosensor and chronoamperometric measurement of fructose:*

254 *a) Plain SPCE; b) SPCE with deposition of nanoparticles in solution; c) SPCE with dried nanoparticles; d) addition*
255 *of 10 μ l FDH, 10 μ l ferricyanide; 20 μ l of solution containing fructose; e) Chronoamperometric measurement*

256

257 *Fig.2. A typical cyclic voltammograms obtained with 0.5 mM ferricyanide in 0.1 M phosphate buffer pH 7.5*
258 *containing 0.1 M potassium chloride using a scan rate of 10 mV s⁻¹: for (A) plain SPCE (B) SPCE-G-COOH.*
259 *Voltammetric conditions: starting potential +0.8 V, switching potential -0.4 V.*

260 *Fig. 3A calibration plots obtained for fructose using a) 1 unit of FDH with a 3 minute incubation time; b) 4 units of*
261 *FDH with a 3 minute incubation time.*

262 *Fig. 3B chronoamperograms obtained with the fructose sensor for various concentrations of fructose: a) 0.00 mM;*
263 *b)0.10 mM; c)0.20 mM; d)0.40 mM; e)0.60 mM; f)0.80 mM; g)1.00 mM. Sensor operation performed with 4 units of*
264 *FDH with a 3 minute incubation time.*

265 *Fig.4A. Typical chronoamperograms obtained with SPCE-G-COOHs for different concentrations of D-fructose:*
266 *a)Apple Juice(AJ), b)0.10 mM, c)0.20 mM, d)0.40 mM, e)0.60 mM and f)0.80 mM. Incubation time at open circuit*
267 *was 180 s, followed by applied potential of + 0.3 V vs Ag/AgCl. The supporting electrolyte was 0.1 M phosphate*
268 *buffer containing 0.1 M potassium chloride.*

269 *Fig.4B. Typical standard addition plot, obtained using chronoamperometric currents measured 20 s after*
270 *application of +0.3 V vs Ag/AgCl*

271

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