

1 **Finite element-based optimisation of an elastomeric honeycomb for impact mitigation in**
2 **helmet liners**

3

4 *Rhosslyn Adams¹, Scott Townsend¹, Shwe Soe², Peter Theobald^{1*}*

5

6 ¹ School of Engineering, Cardiff University, UK

7 ² Department of Engineering, Design and Mathematics, University of the West of
8 England, UK

9

10 * Corresponding author. E-mail: TheobaldPS@Cardiff.ac.uk

11

12 **Keywords**

13 *Honeycomb; optimisation; finite element analysis; impact; helmet; additive manufacturing*

14

15 **Abstract**

16 Finite element simulation was used to analyse the response of an elastomeric pre-buckled
17 honeycomb structure under impact loading, to establish its suitability for use in helmet liners.
18 A finite element-based optimisation was performed using a search algorithm based on a radial
19 basis function. This approach identified optimisation configurations of a pre-buckled
20 honeycomb structure, based on structural bounds subject to impact loading conditions.
21 Furthermore, the influence of objective function, peak acceleration and head injury criterion
22 was analysed with respect to the resultant mechanical behaviour of the structure. Numerical
23 results demonstrate that this class of structure can exceed the performance threshold of a
24 common helmet design standard and minimise the resultant injury index. Experimental testing,
25 facilitated through laser sintering of thermoplastic polyurethane powder, validated the output
26 of the numerical optimisation. When subject to initial impact loading, the fabricated samples
27 satisfied their objective functions. Successive impact loading was performed to assess the
28 performance and degradation. Samples optimised for peak acceleration demonstrated superior
29 performance after stabilisation, relative to their initial response. The culmination of this study
30 establishes a numerical design pathway for future optimisation of candidate structures for head
31 impact protection. Furthermore, the optimised pre-buckled honeycomb structure represents a
32 new class of energy absorbing structure, which can exceed the thresholds prescribed by the
33 design standard.

34 **1. Introduction**

35 Physical activity that includes elevation or speed carries the risk of head injury. Injury risk is
36 mitigated by wearing safety helmets [1], [2], [3]. Whilst cycling is adopted as an exemplar
37 when evaluating new helmets [4], [5] and their use being advocated by the World Health
38 Organisation [6], head injury remains a notable cause of mortality and morbidity in cycling
39 accidents [7], [8]. Indeed, head injury still causes 69-93% of fatal bicycle accidents [9]; hence,
40 new helmet technologies remain of significant social importance.

41

42 Advances in computational modelling and additive manufacturing (AM) have enabled
43 investigation of novel alternative helmet liners that can exceed contemporary materials
44 performance (e.g., Polymeric Foam). *Soe et. al* numerically explored the use of an ordered
45 lattice structure for impact mitigation [10], demonstrating that tailorable energy absorption and
46 thus impact mitigation can be achieved through structural changes. This concept has since been
47 expanded by *Khosroshahi et. al*, who investigated lattice grading schemes and relative density
48 on head injury severity [11], [12]. *Clough et. al* fabricated micro lattice impact attenuators,
49 which afforded greater specific stiffness and densification strain, resulting in a reduction in
50 peak linear acceleration under impact versus stochastically architecture foams [13]. The greater
51 geometric freedom means architected cellular structures hold a notable advantage over
52 stochastic cellular structures. Architected cellular structures with tailorable mechanical
53 properties, therefore, represent a viable route to improving helmet liner performance and
54 ultimately head protection.

55

56 The honeycomb is another example of an architecture cellular structure [14]. Combining
57 properties such as high specific strength and stiffness [15], and excellent impact mitigating
58 properties [16], the honeycomb has become a common design route to achieve lightweight
59 structures with high energy absorption [17], [18]. The adoption of honeycomb structures within
60 helmet design can improve user safety [19], [20]. Localised reinforcement [21], [22], exclusive
61 use [23], or a hybrid combination of foam and honeycombs [24] provide superior performance
62 relative to a monolithic equivalent. In all cases, the principal mechanisms leveraged to mitigate
63 the impact energy are plastic deformation and material fracture. These solutions are unsuitable
64 for applications with potential for multiple (or consecutive) impacts however, as the onset of
65 permanent deformation will diminish helmet performance [25]. Indeed, it is common for
66 consumers to wear a previously damaged helmet despite contrary advice [26]; hence, there is
67 growing motivation in identifying a multi-impact solution [27].

68 In recent years, elastically recoverable honeycomb structures have been investigated due to the
69 potential of repeatable and high specific energy absorption. Furthermore, elastomers can now
70 be additively manufactured, facilitating rapid design exploration of novel structures that are
71 infeasible using traditional methods such as injection moulding [28]. *Bates et. al.*, for example,
72 reported that hexagonal honeycombs additively manufactured from thermoplastic polyurethane
73 achieved recoverable behaviour under cyclic compression, whereby the behaviour of these
74 structures could be tailored by changing the unit cell structure [29], [30]. *Adams et. al*
75 investigated the dynamic response of elastomeric pre-buckled honeycombs, reporting a
76 stabilised yield stress and energy absorption following repeat impact loading [31]. *Townsend*
77 *et. al* investigated the tailorable energy absorption of elastomeric origami-inspired
78 honeycombs, reporting the potential application for helmet liners [32]. *Caccese et. al* is one of
79 few studies describing design optimisation using intelligent search algorithms of elastomeric
80 honeycombs, presenting optimal elastomeric honeycomb structures for head impact mitigation
81 [33]. Adopting a simplified genetic search algorithm, minimum unit cell depth could be
82 identified to achieve a reduced peak acceleration. Loading conditions equivalent to the design
83 certification standards for head protection were not adopted however [34], meaning further
84 investigation is required under these conditions to establish whether this class of structure can
85 satisfy the performance requirement.

86

87 A novel additively manufactured elastomeric pre-buckled honeycomb structure has
88 demonstrated excellent energy absorption capability during quasi-static and dynamic testing
89 over successive loading cycles [31]. This study aims to optimise the honeycomb structure
90 subject to the loading conditions and performance threshold of the design standard for cycling
91 helmets. A numerical approach is outlined that utilises a finite element-based optimisation to
92 identify the optimal honeycomb configuration. Moreover, the influence of varying objective
93 function is also evaluated. Laser sintering of a thermoplastic polyurethane powder is adopted
94 to fabricate the optimal structures, which were experimentally tested under equivalent
95 conditions to enable validation of the numerical approach. Lastly, successive impact testing is
96 carried out to establish the performance degradation over multiple impacts. The outcome of
97 this study is a numerical design pathway for optimisation of candidate structures for impact
98 mitigation.

99

100

101 **2. Materials & Methods**

102 The design of the proposed pre-buckled honeycomb is presented with respect to its structural
103 parameters. The finite element model used to simulate impact loading is then discussed
104 providing the basis for optimisation. The sequential steps of the search algorithm are then
105 described, followed by an overview of the computational sequence. Lastly, the fabrication and
106 testing of optimal honeycombs is detailed.

107 **2.1 Honeycomb structure**

108 A circular pre-buckled honeycomb structure (figure 1) was defined by structural parameters:
109 cell size (w), wall thickness (t), depth (d), circular minor radius (r_1), circular major radius (r_2),
110 and number of folds (f). The aspect ratio (e), hereafter used to describe the eccentricity of the
111 circular cross section of the unit cell, is defined as the ratio of r_1 and r_2 . The fold is based on a
112 cosine function. Computer aided design files for fabrication and simulation were generated
113 using an in-house code written in Python [31].

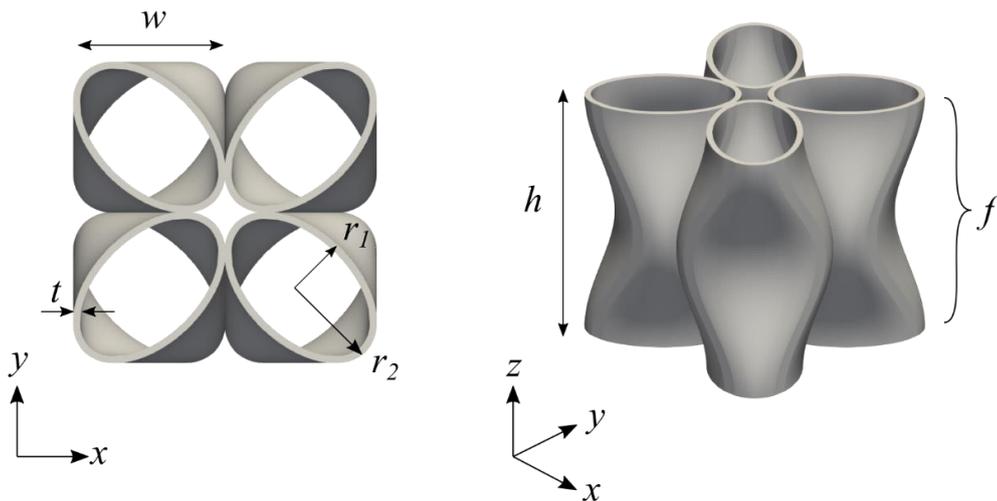


Figure 1: The structural model of the pre-buckled honeycomb unit cell including parameters cell size (w), wall thickness (t), depth (d), circular minor radius (r_1), circular major radius (r_2) and number of folds (f).

114 **2.2 Finite element model**

115 Finite element analysis (Abaqus Explicit 2019; Dassault Systems, France) was performed to
116 replicate the shock absorption test from the cycling helmet design standard EN1078 [35]. The
117 model comprised a deformable honeycomb comprising of two unit cells positioned between
118 two analytically rigid plates as illustrated by figure 2.

119

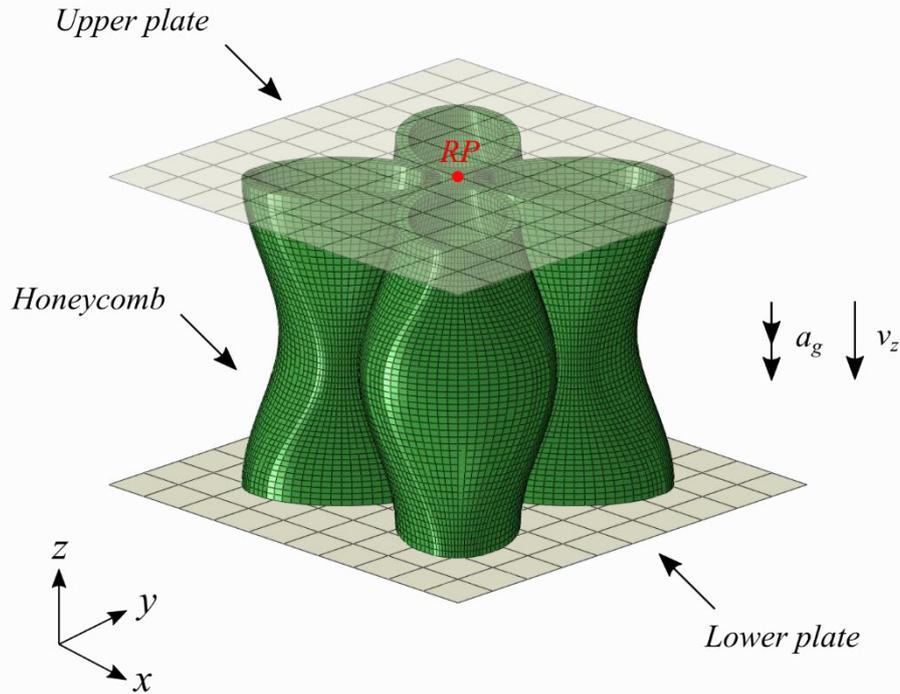


Figure 2: The finite element model of the pre-buckled honeycomb comprising of two unit cells positioned between an upper and lower rigid plate. The upper plate is assigned a pre-impact velocity and point mass, whilst the lower is fixed.

120

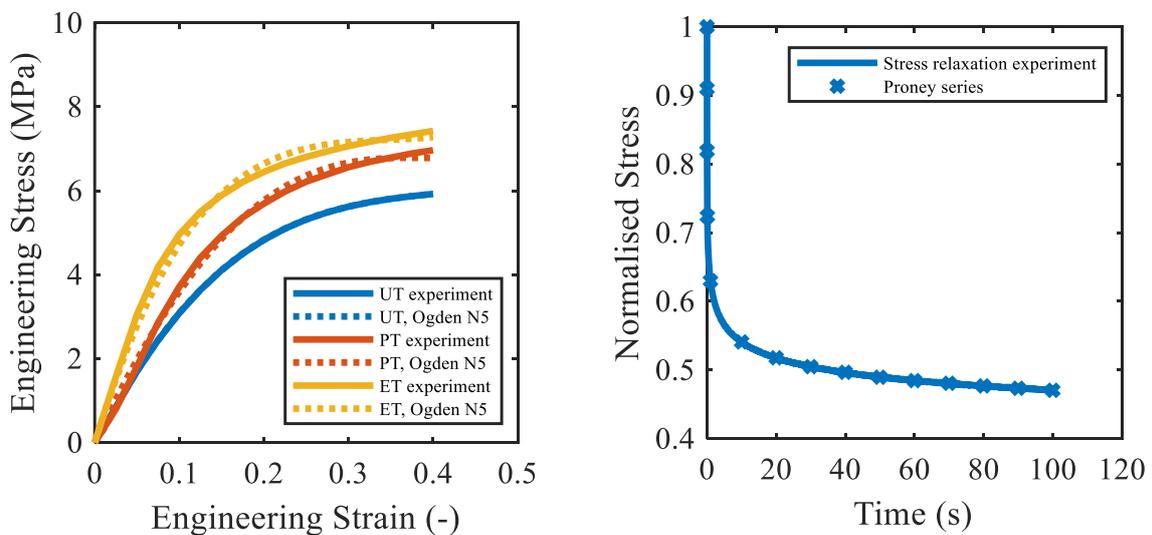
121 The lower plate was assigned an encastre boundary condition and the upper plate a point mass
 122 of 4.7kg, equivalent to a size J headform [36]. Pre-impact velocity of $v_z = 5.42\text{ms}^{-1}$ was adopted
 123 from the design standard, whilst global acceleration due to gravity, $a_g = 9.81\text{ms}^{-2}$ was
 124 assigned to the entire model. This represents the experimental setup (section 2.5) enabling
 125 validation of the numerical outcome, whilst simplifying the anticipated crushing between the
 126 head and the liner under impact.

127

128 An efficient periodic boundary condition model alleviated the computational cost of multiple
 129 full-scale simulation. In the model, the 2 x 2 honeycomb configuration has zero displacement
 130 in the X and Y axes along the perimeter nodes. The lower plate boundary conditions
 131 remained the same, whilst the upper plate point mass was scaled by 0.25, proportional to the
 132 kinetic energy, to account for load distribution over a quarter of the projected area. Previous
 133 work validated this approach, reporting it as comparable to 4 x 4 honeycomb array under impact
 134 loading [31].

135

136 An eight-node brick element with hexahedron shape type, reduced integration and hourglass
 137 controlled was utilised (C3D8R). The mesh density was selected so that there were two
 138 elements across the wall thickness to mitigate against shear locking; mesh independence
 139 studies identified diminishing gains using greater than two elements. A global friction value of
 140 1.0 was used to emulate the anticipated friction that arises from self-contact of the elastomeric
 141 material, in accordance with similar studies [31], [32]. Although this global friction is not likely
 142 to represent the surface contact between the plates and honeycomb, it is considered an
 143 acceptable simplification due to the relatively small contact area. Luvosint was adopted as the
 144 base material, a thermoplastic polyurethane utilised in additive manufacturing (e.g., laser
 145 sintering), with a density of 1200kg/m^3 . Material behaviour was characterised under uniaxial,
 146 planar and equiaxial tension, as well as single step stress relaxation and is described in figure
 147 3. The numerical material model was validated under quasi-static and dynamic, isolated and
 148 mixed deformation testing [37], [38]. An isotropic Ogden N5 material model was used to
 149 represent the non-linear hyperelastic behaviour, which was then augmented with a linear
 150 viscoelastic material model, Prony series, to represent the rate dependant behaviour (material
 151 model coefficients are reported in the appendix, table A1 and A2 respectively). Initial
 152 honeycomb impact tests indicated no obvious structural fracture nor material plasticity;
 153 therefore, fracture and damage was not considered in the numerical simulations. Furthermore,
 154 whilst it is well known that additive manufacturing's layer by layer process yields a degree of
 155 local anisotropy with respect to the build direction, this was not considered in the numerical
 156 analysis as the mechanical behaviour is recognised to be less sensitive when exposed to
 157 compressive loads in line with the build axis [39].



(a) Uniaxial (UT), planar (PT) and
equibiaxial tension (ET) experiment
compared to material model

(b) Stress-relaxation experiment compared
to material model

Figure 3: Mechanical behaviour of the sintered Luvosint under three modes of deformation and stress relaxation used in the calibration of the hyperelastic and linear viscoelastic model respectively. Adopted from [37].

158

159 A 15ms simulation time was used to sufficiently capture the entirety of the impact event.
160 Reaction force, linear acceleration, and velocity, as well as displacement in the Z-axis
161 was recorded with respect to time and extracted from the reference point located on the upper
162 surface. This was then used to calculate the dynamic stress and strain at the reference point.
163 Stress was calculated by dividing the reaction force by the projected cross-sectional area and
164 strain by normalising the plate displacement by the honeycomb height. The recorded data was
165 further treated with a low pass Butterworth filter that had a 1000Hz cut-off frequency.
166 Head injury criterion (HIC) was also calculated, using equation (1), to establish the relative
167 severity of the resultant acceleration [40]. Since there was no rotational kinematics induced
168 during the impact, rotational severity indexes were not considered.

169

$$170 \quad HIC = \max \left[\frac{1}{t_2 - t_1} \int_{t_1}^{t_2} a(t) dt \right]^{2.5} (t_2 - t_1) \quad (1)$$

171

172

173 **2.3 Optimisation**

174 To identify the ideal honeycomb parameters for impact mitigation, numerical optimisation was
175 performed based on a finite number of simulations using the surrogate optimisation algorithm
176 available in MATLAB's Optimisation Toolbox (MathWorks, United States). The surrogate
177 optimisation algorithm, which is based on a radial basis function [41], was adopted over other
178 search algorithms available in MATLAB, such as genetic, particle swarm or simulated
179 annealing due to its capability of accurately modelling arbitrary functions, handling scattered
180 training points in multiple dimensions and requiring fewer iterations [42]. Moreover, since it
181 is a non-gradient based solver, it is more appropriate for problems that include discontinuities
182 due to self-contact. Lastly, it is more suited to time-consuming objective functions, such as
183 finite element problems, as it is proven to converge to a global optimum for bounded problems.

184

185 The surrogate optimisation algorithm occurs over multiple steps, as illustrated by figure 4.
186 Initially, quasi-random points are sampled throughout the design space, with the objective
187 function evaluated following each successful design point simulation. The surrogate, which
188 approximates the relationship between each design point and the objective function, is then
189 constructed by interpolating a cubic spline with a linear tail through the sampled points. Next,
190 the algorithm searches for the minimum. New values are sampled within the design space
191 around the incumbent value. A merit function is evaluated subject to the surrogate model values
192 at these points, as well as the distance between them and the points where the objective function
193 has already been evaluated. The best point, based on its merit function, is simulated and the
194 objective function evaluated. The surrogate model is then updated to reflect the new
195 information. This cycle repeats for a finite number of iterations where the fidelity of the
196 surrogate model improves. Upon convergence, the surrogate model is reset, and new random
197 samples selected to ensure the design space is fully explored. Once the maximum number of
198 iterations is reached, the minimum point can be identified.

199

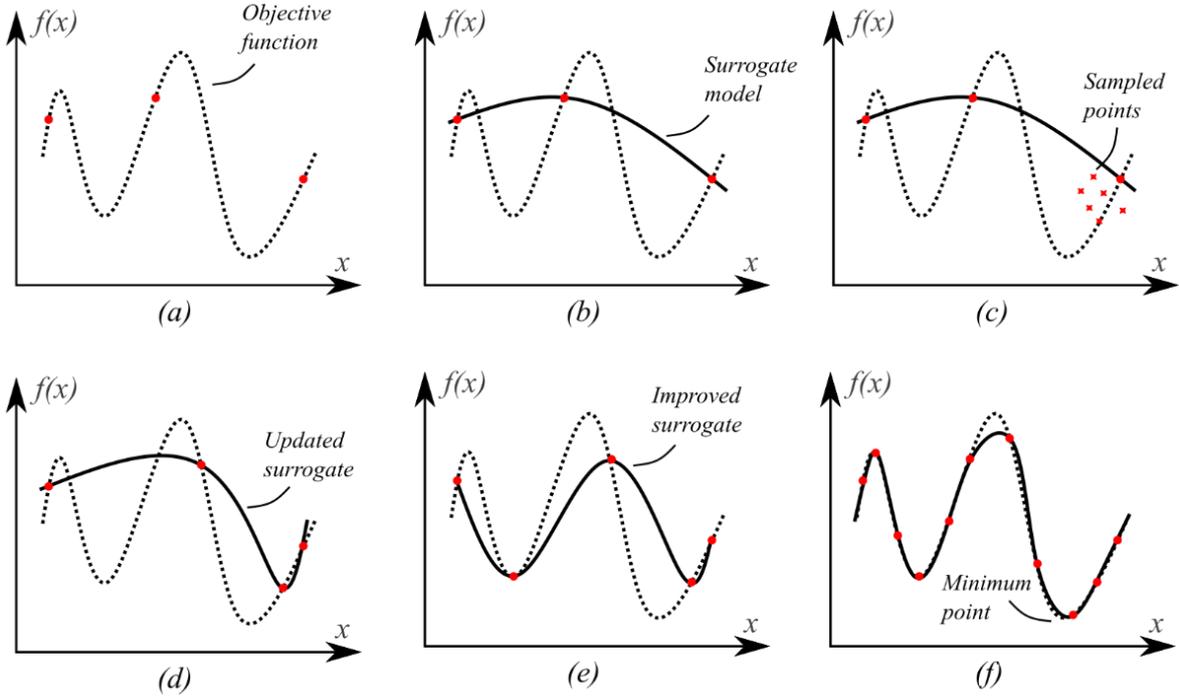


Figure 4: The optimisation steps for construction of the surrogate response used by the search algorithm for an increasing number of sampled finite element simulations including, (a) random sampling, (b) surrogate construction, (c) merit function analysis, (d) best point simulated, (e) surrogate model updated and (f) final surrogate model approximation.

200

201 The objective function used in this optimisation was adopted from the cycle helmet design
 202 standard (EN1078), which defines an acceptable shock absorption threshold. The standard
 203 mandates that, for a singular impact, the resultant acceleration shall not exceed 250g [35].
 204 Consequently, the objective function was defined by equation (2).

205

$$206 \quad f(x_d) = \frac{J_{calc}}{J_{crit}} \quad (2)$$

207

208 Where $f(x)$ is the objective function, x is the structural parameter vector, J_{calc} , is the calculated
 209 objective function recorded during the simulation, normalised by J_{crit} a critical threshold value.
 210 The optimisation problem is therefore defined by the number of structural parameters, x , the
 211 constructed surrogate model, and subject to structural parameter limits described as follows:

212

213 *Find: t, e*

214 *Minimise: $f(x)$*

215 *Subject to: $w = 12.5mm, d = 25.0mm, 0.8mm \leq t \leq 1.4mm, 0.6 < e < 0.8, f = 1.0$*

216

217 To utilise the optimisation approach, a computational procedure was developed. As illustrated
218 by figure 5, Matlab, Python and Abaqus, were utilised to execute the structural optimisation.

219 Initially, user-specified inputs such as maximum number of iterations, loading conditions

220 (mass and velocity) and structural parameter limits were set. The optimisation search algorithm

221 was then initiated using Matlab. The structural parameter vector was parsed, and a Python

222 script was called that meshed the structure. A secondary script consisting of indigenous Abaqus

223 macros imported the newly meshed configuration, applied boundary conditions and wrote the

224 simulation job file. Once the new job file was written, Matlab executed the job. Upon

225 completion of the simulation, the result file was automatically analysed and filtered using

226 another Python script, before being imported into Matlab which calculated the objective

227 function. This procedure was then repeated where the structural parameter vector changes with

228 respect to the calculated objective function. Once the user prescribed iteration limit was

229 reached, the procedure ends.

230

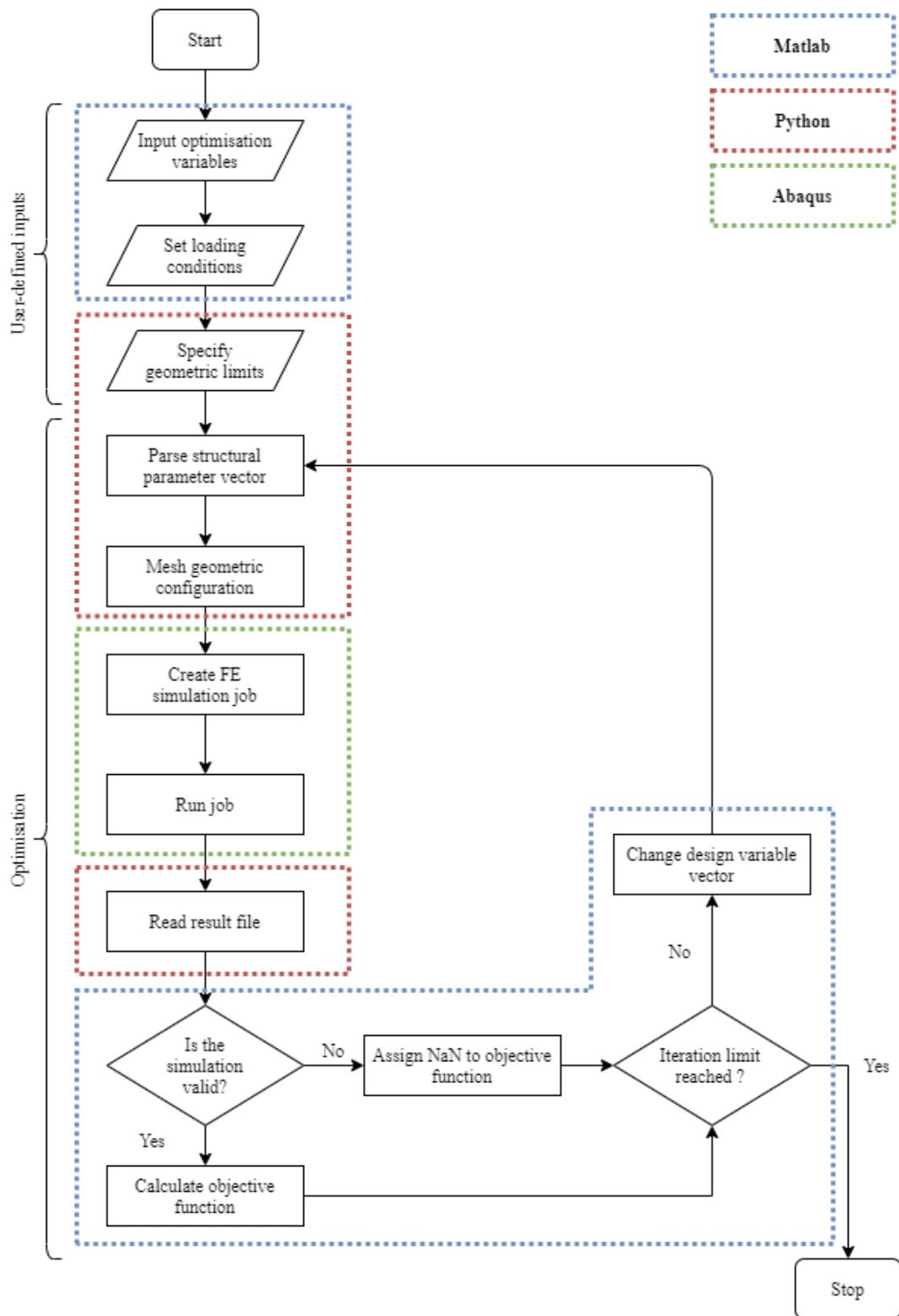


Figure 5: The outline of the computational procedure indicating the software used during each step of the optimisation (oval = start/end, parallelogram = input/output, rectangle = process, diamond = decision).

233 **2.4 Honeycomb fabrication**

234 Additive manufacturing was employed to fabricate the honeycombs identified through the
235 optimisation. Figure 6 illustrates the computer aided design files, generated using a python
236 script, were converted to .stl file format for interpretation by the laser sintering machine.
237 Fabrication was sub-contracted to a specialist third party, building parts from Luvosint X92A-
238 1 (Lehmann & Voss & Co; Hamburg, Germany) a thermoplastic polyurethane powder
239 described in section 2.2. A contouring scan mode was leveraged with a minimum layer
240 thickness in the z direction was set to 0.1mm. Post processing was performed using
241 compressed air to remove excess unsintered powder. Build accuracy was assessed by
242 measuring finished parts using a Vernier Calliper (Absolute AOS Digimatic, Mitutoyo, Japan),
243 for comparison to the intended design values.

244

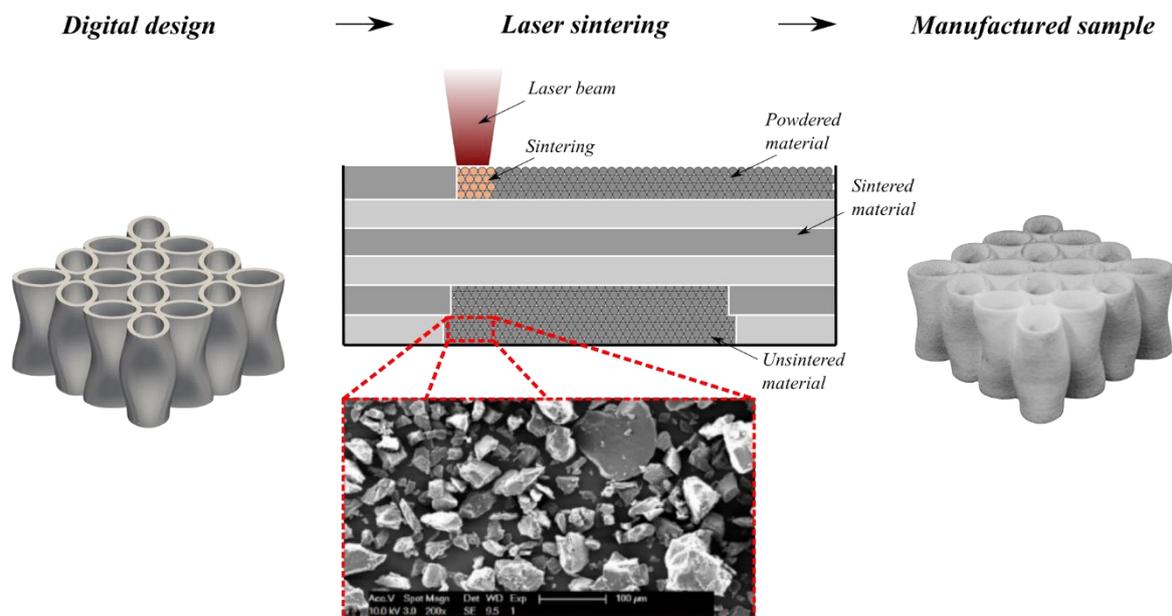


Figure 6: The fabrication method for the optimal honeycomb design including digital design, laser sintering overview and final part. Scanning electron imagery of Luvosint powder has been adopted from [43]

245

246

247 **2.5 Experimental validation**

248 Fabricated honeycombs were subjected to dynamic impact loading, to validate the results of
249 the numerical optimisation procedure. This was performed using a monorail shock absorption
250 testing facility (model: 1002 MAU 1006/CF/ALU; AD Engineering, Italy) (figure 7). Each
251 honeycomb was taped to the upper platen of the drop carriage, which was designed specifically
252 to have an equivalent mass to a size J headform (4.7kg). The carriage was then wire-guided,
253 under free-fall, onto a steel anvil that had a 50kN load cell positioned within it. Each sample
254 was subjected to an initial impact velocity of 5.42m/s validated through use of a light gate.
255 Data was recorded at 50,000Hz and treated with a low pass Butterworth filter that had a
256 1000Hz cut-off frequency. The line of impact was out-of-plane to the build orientation. All
257 testing was performed in ambient conditions.

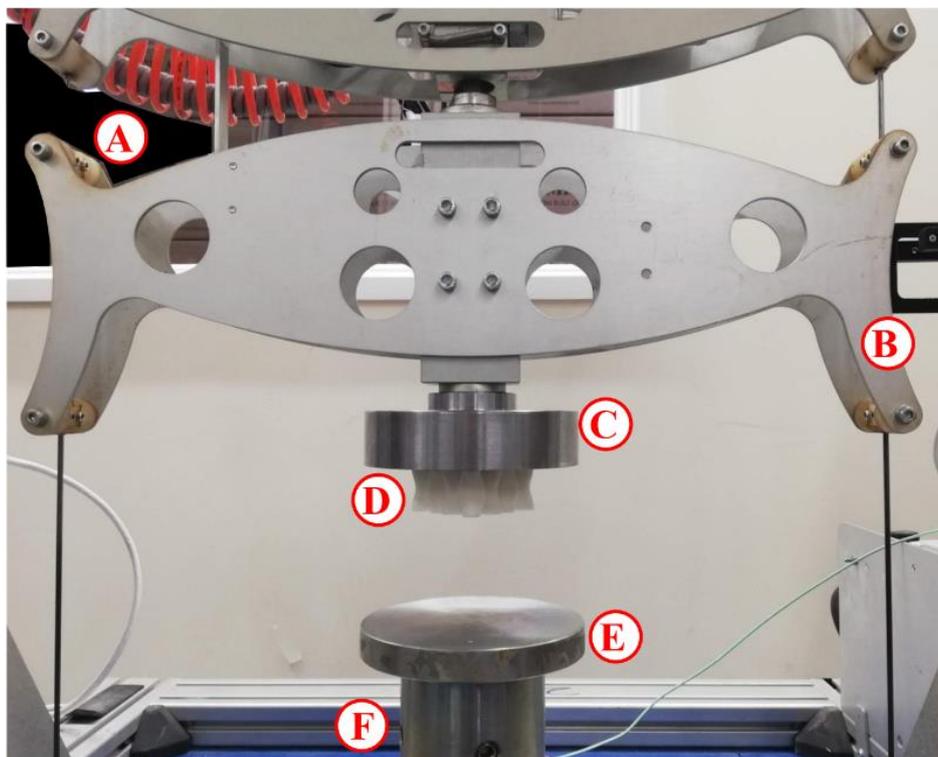


Figure 7: The experimental setup for impact testing of the optimised honeycomb samples including drop carriage (A), light gate (B), upper plate (C), honeycomb sample (D), lower plate (E), load cell (F).

258

259

260 **3. Results**

261 In this section, the results from the numerical optimisation are presented. The variation in
262 honeycomb impact behaviour is reported relative to the number of function evaluations as well
263 as changing the objective function. Variation in objective function relative to structural
264 parameters is also discussed. Following, fabricated samples are subject to experimental testing
265 to validate the outcome of the numerical optimisation. Lastly, testing is carried out over
266 successive repeats to explore the multi-impact behaviour and performance degradation of the
267 fabricated honeycombs.

268

269 **3.1 Optimisation**

270 Figure 8 reports the variation in the objective function, peak linear acceleration (PLA), for each
271 evaluation relative to the acceptable 250g limit during the optimisation. The optimisation
272 procedure successfully satisfied the objective function yielding a response less than 250g. The
273 first 20 evaluations are randomly sampled yielding a variation in objective function between
274 419.7 and 158.0g. The minimum value reported in the random sample was at iteration 9. This
275 represents a relative reduction in the objective function by 36.8%. The optimal solution was
276 identified during the first surrogate, within the adaptive sampling phase between iterations 20
277 and 75. The minimum solution reported was 140g at the 56th evaluation representing a further
278 reduction by 11.4% compared to the best point of the random sample. To ensure that the current
279 best point was the global minimum, the surrogate model was reset after the 75th iteration and
280 random sampling was undertaken to construct a new surrogate. The surrogate reset failed to
281 achieve an improvement on the best point from the first surrogate. Similarly, a third and final
282 reset (started at 125th iteration) also failed to achieve an improvement, although the procedure
283 was terminated prior to reaching adaptive sampling as the maximum number of iterations had
284 been exceeded ($i_{\max} = 150$).

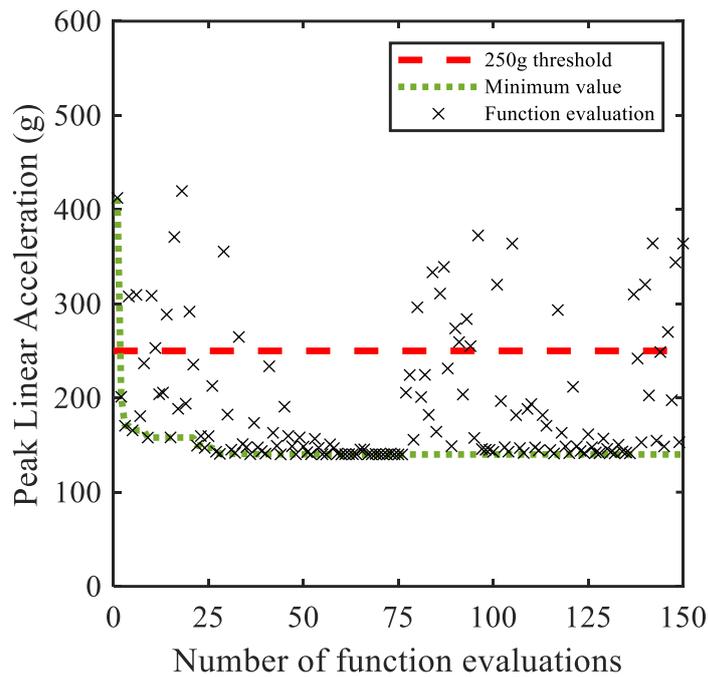


Figure 8: The variation in the objective function, peak linear acceleration, for each function evaluation relative to a threshold of 250g

285

286 Figure 9a – 9c illustrates the changing resultant acceleration and mechanical behaviour of the
 287 honeycomb during the optimisation procedure. Comparison is made to the acceptable shock
 288 absorption threshold of the design standard, as well as the failure criterion for skull fracture
 289 [44]. Iterations 1, 14 and 56, of the first surrogate model, are reported as they demonstrate two
 290 characteristic behaviours and the optimal result. Iteration 1 represents an overly compliant
 291 response. As the structure begins to deform, buckling occurs at a relatively low stress, initially
 292 resulting in a low acceleration. As the structure proceeds through the plateau region, the
 293 structure fails to sufficiently mitigate the kinetic energy of the impactor. Consequently, the
 294 structure begins to densify yielding a large and rapid increase in acceleration, exceeding the
 295 acceptable threshold, as the impact is mitigated through compression of the base material. The
 296 duration of the impact occurs over 9ms, reaching a PLA of 412g, and a peak stress of 7.6MPa.
 297 Conversely, iteration 14 represents an overly stiff response. The structure deforms at a high
 298 stress, yielding a high initial acceleration, which exceeds the permissible threshold. By the time
 299 the structure buckles, entering the non-linear region before the plateau phase, the kinetic energy
 300 of the impact has been mitigated leading towards a response which is over in less than 6ms
 301 reaching a PLA of 288g, and a peak stress of 5.3MPa. Iteration 56 represents the optimal
 302 solution. The response effectively mitigates the kinetic energy prior to reaching the onset of

303 densification, without exceeding the 250g threshold. Buckling occurs at a stress that is below
 304 the acceptable threshold; whilst structural stress-softening is observed, acceleration remains
 305 nearly constant throughout.

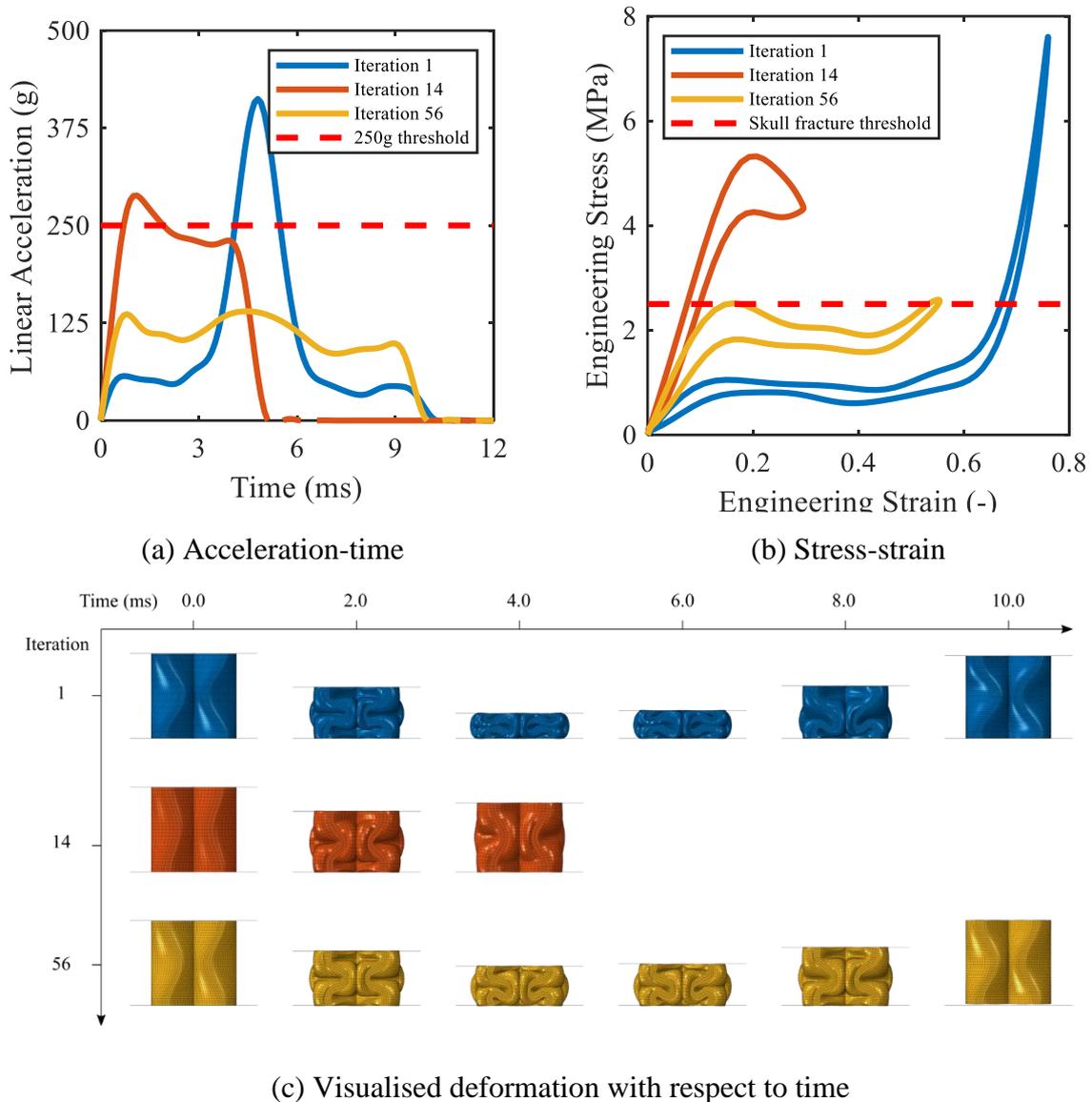


Figure 9: The simulated response for iterations 1, 14 and 56 for the optimisation where PLA was the objective function

306

307 Figure 10 further examines the data recorded in the optimisation procedure. In addition to PLA,
 308 HIC was calculated at each function evaluation; the variation in PLA and HIC is reported at
 309 each function evaluation. The data features two trends constructed in a slanted 'V-shape'.
 310 Firstly, the left-hand side trend ranges between 140 to 412g, within which the value for HIC
 311 varies between 1129 to 3024. Conversely, for a similar PLA range, the associated right-hand
 312 HIC values range from 1129 to 5658. These two trends meet at a point of intersection located

313 at the bottom left-hand corner. The density of function evaluations in this region, compared to
 314 the others, is indicative of the location of the identified minimum. The ‘V-shape’ formulation
 315 of data reports an interesting feature, where points of equivalent PLA have markedly different
 316 HIC. One such instance is reported in figure 11a and 11b, which compares the acceleration-
 317 time and mechanical behaviour of these two points. Similar behaviour to that observed in 9a
 318 and 9b is observed i.e., a stiff structure that mitigates the kinetic energy prior to reaching the
 319 plateau, versus a compliant structure that mitigates kinetic energy by deforming within the
 320 plateau and densification region. Interestingly the search algorithm qualifies both results
 321 equally based on the PLA reported, however, the calculated HIC values are markedly different.
 322 Notably, the HIC value for the stiff structure is 114.1% greater than the compliant structure.
 323 Since the search algorithm examines these two responses equally, a greater number of iterations
 324 is required to attain the optimum solution. In both cases the requirement of the design standard
 325 (PLA < 250g), and thus objective function have been satisfied; however, owing to the
 326 significance of HIC as an injury severity index, it is prudent for further optimisation to consider
 327 HIC as the objective function.

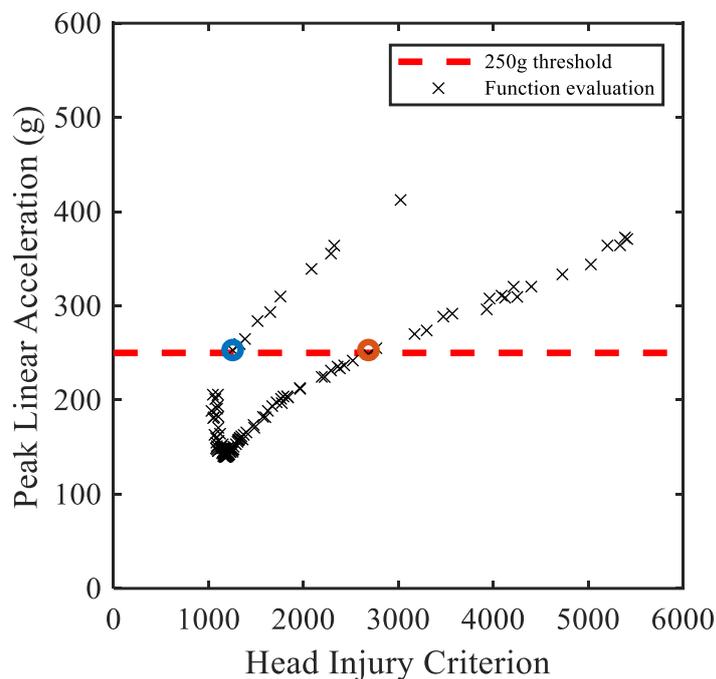


Figure 10: The variation in peak linear acceleration and head injury criterion at each function evaluation. Two points of equivalent PLA are indicated on the plot to be used in reference to figure 9.

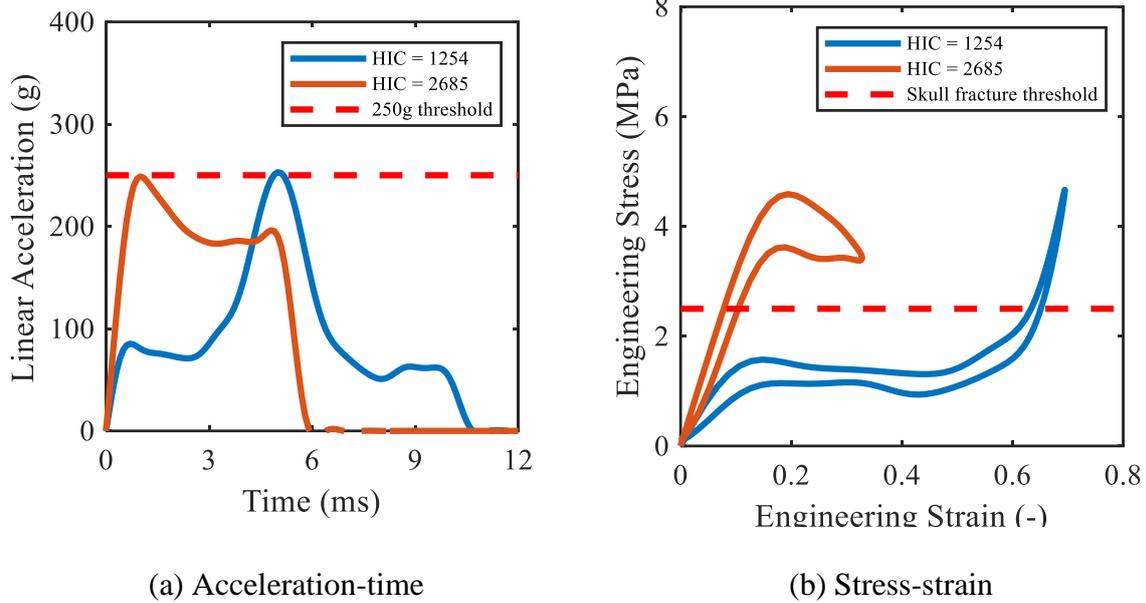


Figure 11: The comparison of impact response and mechanical behaviour of iteration 11 and 136, identified from figure 8, response when yielding the same peak linear acceleration

328

329 Figure 12 compares the objective function relative to the structural parameters, wall thickness
 330 and aspect ratio. The contour plot illustrates a band of minimum peak linear acceleration,
 331 neighboured equally either side by areas of increasing values indicating that the results are
 332 forming a valley shape where the minima is located within the gully. The two localised
 333 clusters of function evaluations are representative of the completed adaptive sample phases.
 334 The optimal values found for each surrogate were within 1% of each other. This suggests that
 335 for the pre-buckled honeycomb structure there is a band of optimal values for various
 336 combinations of wall thickness and aspect ratio as indicated by the dashed lines. Within this
 337 band of near contact performance for decreasing aspect ratio an increase in wall thickness is
 338 required to mitigate the impact.

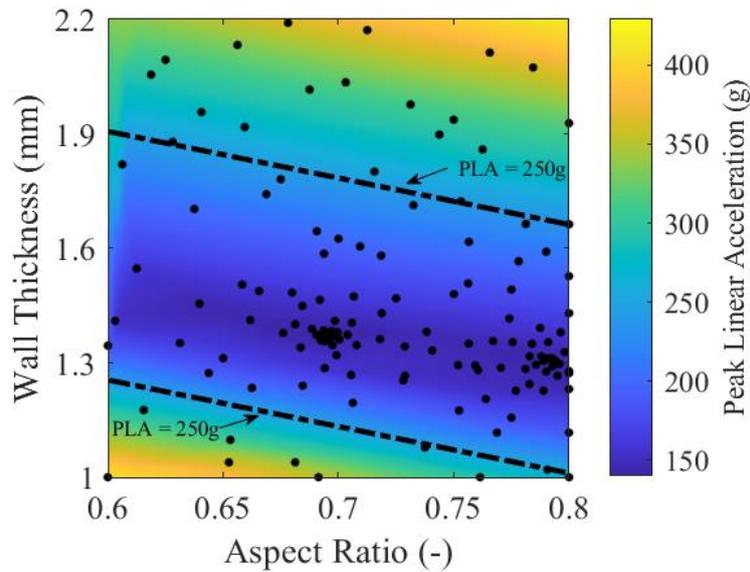


Figure 12: The variation in peak linear acceleration relative to wall thickness and aspect ratio when the objective function is set to PLA. Each function evaluation is indicated by a black point.

339

340 To examine the influence of objective function, HIC was used in a secondary optimisation.
 341 Considering equation (1), the objective was calculated and normalised by a value of $HIC =$
 342 1574, equivalent to an abbreviated injury score (AIS) of 4, whilst all other optimisation and
 343 structural parameters remained the same. Figure 13 reports the variation in objective function,
 344 HIC, for each evaluation relative to the new acceptable threshold during the optimisation. The
 345 optimisation procedure successfully satisfied the objective function yielding a response with a
 346 HIC less than 1574. The first 20 evaluations are randomly sampled yielding a variation in HIC
 347 between 5412 and 1050. The minimum value reported in the random sample was at iteration
 348 7. This represents a reduction in the objective function by 33.3%. The minimum solution was
 349 identified during the adaptive solution between iterations 20 to 85. The minimum solution
 350 reported was $HIC = 1029$ at the 48th evaluation representing a reduction of 2.0% compared to
 351 the best point of the random sample. Subsequent function evaluations do not yield an improved
 352 result. After the 90th function evaluation the surrogate model is reset and random sampling
 353 occurs again to construct the surrogate model, however, this search does not attain
 354 improvement.

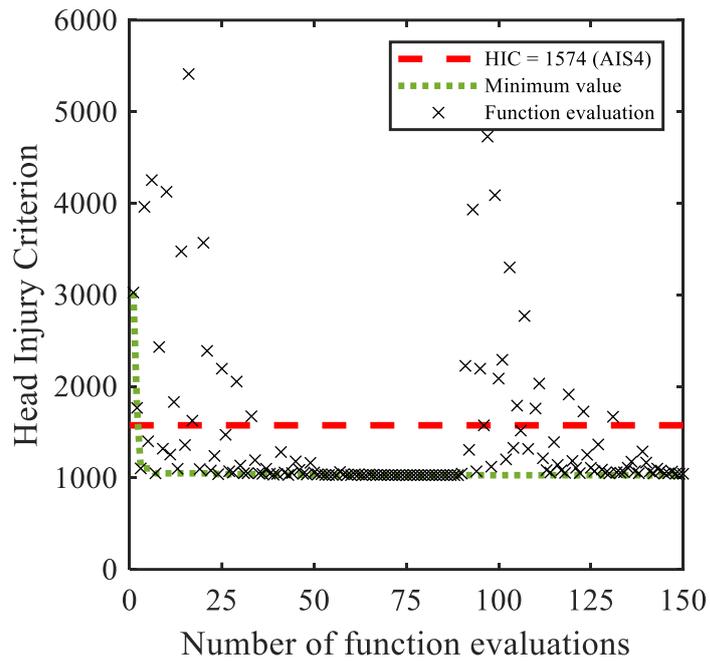


Figure 13: The variation in the objective function, head injury criterion, for each function evaluation relative to a threshold of 1574.

355

356 Figure 14 compares the objective function, HIC, relative to the structural parameters of wall
 357 thickness and aspect ratio. The contour plot illustrates a similar trend to figure 12. Figure 15
 358 compares the optimal results from the PLA and HIC optimisation, hereafter referred to as
 359 PLA_{opt} and HIC_{opt} respectively. The objective function has a notable influence on the resultant
 360 mechanical response of the honeycomb. Specifically, the PLA_{opt} favours a higher yield and
 361 plateau stress than HIC_{opt} . Conversely HIC_{opt} favours a lower yield stress and takes advantage
 362 of densification. The reported PLA and HIC values for each optimal are reported in table 1.

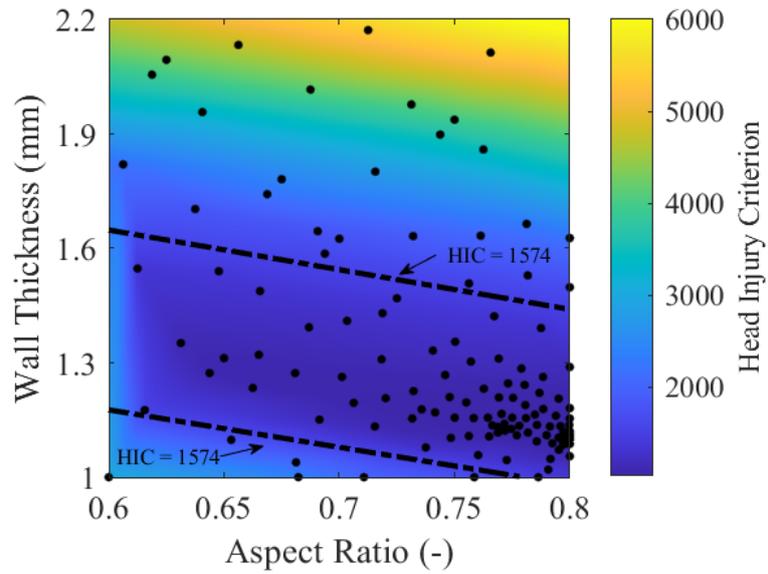


Figure 14: The variation in head injury criterion relative to wall thickness and aspect ratio when the objective function is set to PLA. Each function evaluation is indicated by a black point

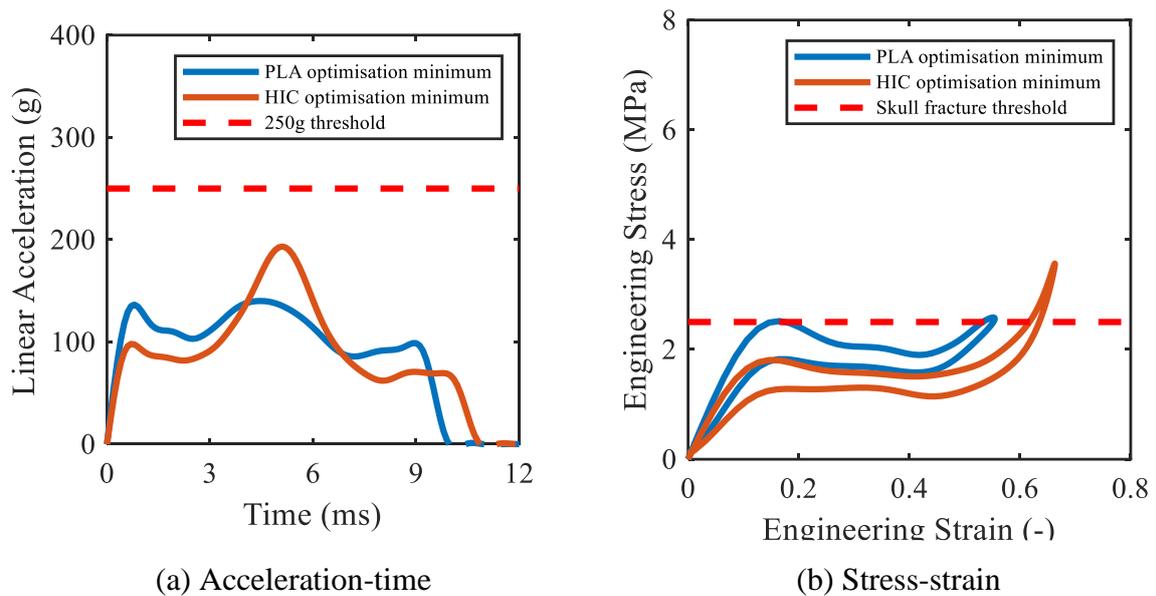


Figure 15: Comparison of mechanical behaviour for optimal honeycombs based on an objective function of PLA and HIC.

363 Table 1: Structural and performance parameters for the optimal values for both objective
364 functions.

Objective function	Cell width (mm)	Wall thickness, t (mm)	Aspect ratio, e	Number of folds, f	PLA (g)	HIC
PLA	12.5	1.37	0.70	1.0	140.0	1174
HIC	12.5	1.11	0.80	1.0	193.2	1029

365 **3.2 Experimental validation**

366 **Sample inspection**

367 As previously discussed, the optimised honeycomb structures were fabricated using laser
368 sintering. The wall thickness was measured across 16 positions as well as overall length, width
369 and height for each specimen. The values were then averaged and compared to the CAD models
370 as reported by table 2. Visual inspection of the samples did not identify any defects due to
371 residual stresses from the sintering process, such as warping or curling [45].

372

373 Table 2: Recorded dimensions of the fabricated honeycomb samples, difference from design
374 values provided in brackets.

Label	Average wall thickness (mm)	Sample length (mm)	Sample width (mm)	Sample height (mm)
PLA _{opt}	1.42 (0.05)	50.05 (0.05)	50.02 (0.02)	25.04 (0.04)
HIC _{opt}	1.06 (-0.05)	49.62 (-0.38)	49.32 (0.68)	26.08 (1.08)

375

376 **Single impact**

377 Impact loading was performed on the fabricated honeycombs to demonstrate that the
378 optimisation process yields structures which satisfy their objective functions. Figure 17a and
379 17b reports the acceleration-time data for the PLA_{opt} and HIC_{opt}. The PLA_{opt} solution satisfies
380 its objective function, yielding a PLA value of 232.2g. This represents a relative decrease of
381 7.1% compared to the threshold value. The PLA_{opt} solution also satisfies the HIC objective
382 function, yielding a value of 1274 and representing a relative decrease of 19.1%. The HIC_{opt}
383 solution also satisfies its objective function, yielding a HIC value of 1085, which is a relative
384 decrease of 31.1% compared to the threshold value. The HIC_{opt} solution, however, did not
385 satisfy the PLA_{opt} threshold. The recorded PLA was 258.6g which exceeds the threshold value
386 by 3.4%.

387

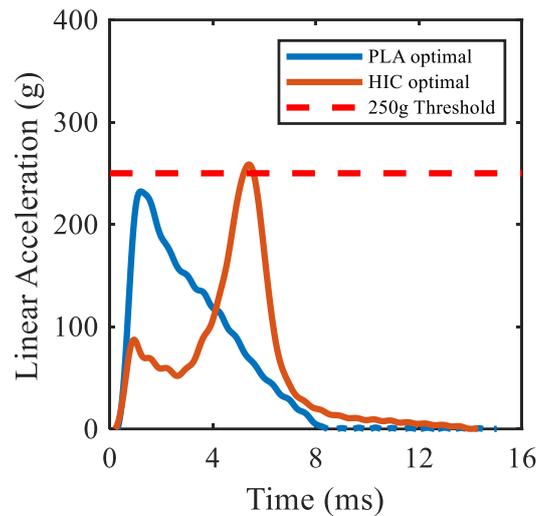


Figure 17: Experimental data of single impact loading for PLA and HIC optimised solutions

388

389 **Repeat impact**

390 Following the initial single impacts, each sample was subjected to 4 additional repeat impacts
 391 at 1-hour intervals to characterise the multiple loading behaviour of the optimal structures.
 392 Figure 18a and 18b reports the acceleration-time data for samples of PLA_{opt} and HIC_{opt} with
 393 respect to the first, third and fifth repeat impact. Moreover, figure 18c and 18d reports the PLA
 394 and HIC values reported with respect to all repeat impacts.

395

396 The PLA_{opt} solution was optimised with respect to an objective function threshold of PLA <
 397 250g. Following the second impact, the PLA recorded was 172.3g representing a relative
 398 reduction of 25.8%. For an increasing number of impacts an improvement in performance was
 399 observed. For impacts 3 – 5, a successive relative reduction of 8.5%, 1.8% and 2.5% is
 400 observed. Moreover, repeat impacts 4 and 5 represent a stabilised response when compared to
 401 impacts 1 – 3 which yields less variation and a more predictable response. Comparing the
 402 performance of the final impact (number 5), the reported value is 39.6% less than the objective
 403 function threshold (250g). The PLA_{opt} results also satisfies the HIC_{opt} objective function for
 404 repeat impacts. Similar to the PLA trends, the reported HIC values decreased for increasing
 405 number of impacts. For a single impact the reported HIC value was 1274. Following the second
 406 impact, the HIC value recorded was 945 representing a relative reduction of 25.8%. For impact
 407 3 – 5, a successive reduction of 3.5%, 2.0% and 1.0% was observed. Comparing the

408 performance of the final impact (number 5), the reported value was 29.9 % less than HIC_{opt}
409 objective function threshold.

410

411 The HIC_{opt} solution was optimised with respect to an objective function of $HIC < 1574$.

412 Following the second impact, the HIC recorded was 2723 representing a relative increase of

413 150.1%. For an increasing number of impacts a common trend of deteriorating performance is

414 observed. For impacts 3-5, a successive increase of 32.6%, 12.1% and 8.9% is reported.

415 Comparing the performance of the final impact (number 5), the reported value is 306.0%

416 greater than the critical value. As previously discussed in the analysis of single impact

417 behaviour, the HIC_{opt} solution does not satisfy the PLA_{opt} objective function. For the first repeat

418 impact, the PLA recorded was 446.2g representing an increase of 72.5%. For an increasing

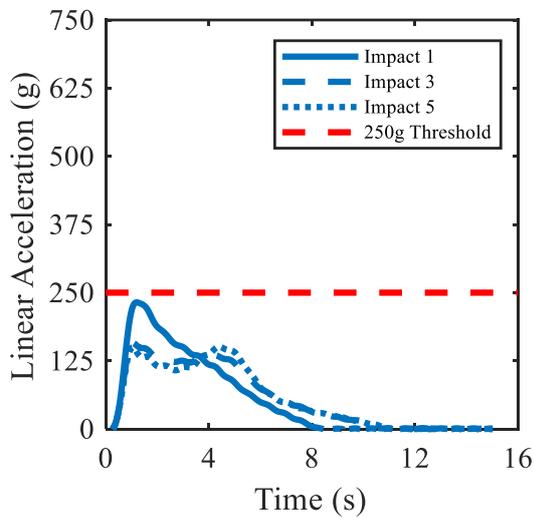
419 number of impacts a common trend of deteriorating performance is observed. For impacts 3 –

420 5, a successive increase of 19.8%, 7.3% and 5.2% of PLA is reported. Comparing the

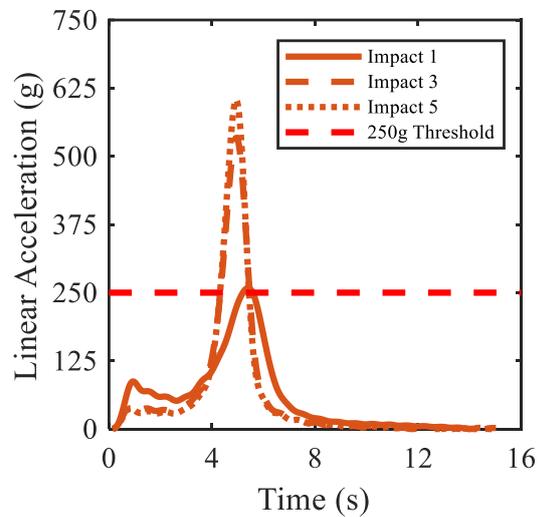
421 performance of final impact (number 5), the reported value is 141.3% greater than the critical

422 value (250g).

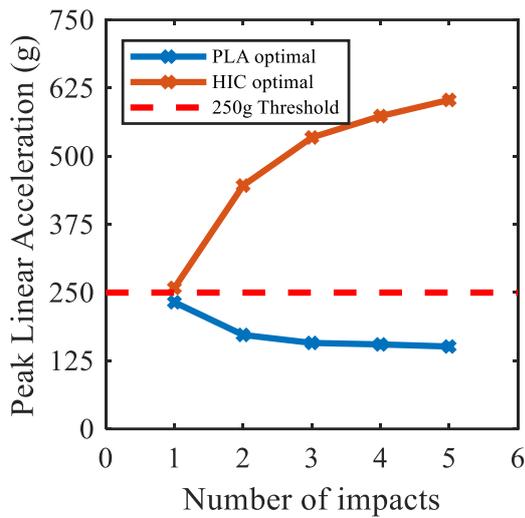
423



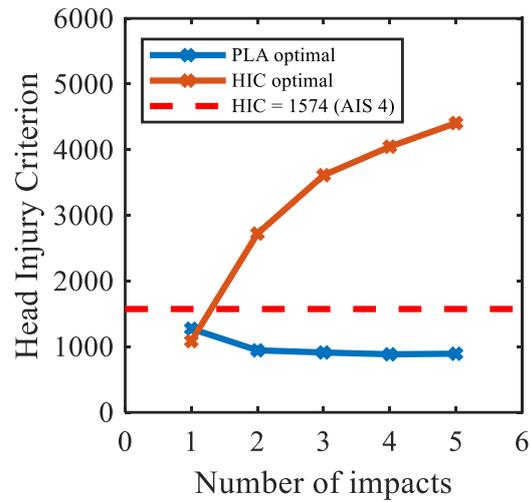
(a) PLA_{opt} acceleration-time



(b) HIC_{opt} acceleration-time



(c) Comparison of PLA



(d) Comparison of HIC

Figure 18: Experimental comparison of repeat impact loading for PLA and HIC optimised solutions

424

425 4. Discussion

426 In this section, the effect of changing objective function is qualitatively analysed relative to the
 427 mechanical behaviour of the honeycomb. Following, experimental phenomena observed are
 428 related to structural and material-based energy absorption mechanisms of the honeycomb.
 429 Next, limitations in performance are reported before expanding on future applications of the
 430 optimisation process.

431 Finite element simulations were employed to obtain the resultant acceleration of the
 432 parametrised pre-buckled honeycomb structure when subject to impact loading. The surrogate
 433 optimisation algorithm from the MATLAB toolbox was used to analyse the results of FE
 434 simulation response relative to the design space. It was shown that the novel circular pre-
 435 buckled honeycomb design can minimise PLA and therefore satisfy the requirements of the
 436 design standard, but this was achieved at the expense of the HIC index. Varying the objective
 437 function from PLA to HIC resulted in notable differences in honeycomb response. The PLA
 438 optimal favoured a high yield and plateau stress, ensuring that the impact energy had been
 439 mitigated prior to entering densification, avoiding the characteristic large and rapid increase in
 440 acceleration. In contrast, the HIC optimal favoured a lower yield and plateau stress, resulting
 441 in densification of the structure. Since the structure yields at a lower comparative stress, the
 442 resultant acceleration is reduced in comparison to the PLA optimal. Once the structure

443 densifies, however, the resultant acceleration exceeds that of the PLA optimal. This reduces
444 the time of exposure to injurious levels of acceleration [46].

445

446 Experimental testing aimed to validate the numerically identified optimal configurations. Both
447 structures, when tested experimentally, satisfied their respective objective function, however,
448 the reported results did not match the numerical analysis. The HIC_{opt} configuration adopts a
449 low yield stress which results in a reduced linear acceleration for a large proportion of the
450 impact. It, however, takes advantage of the densification region to mitigate residual impact
451 force for short periods at high acceleration. Consequently, there is a small operational window
452 with which this structure works optimally. Variance in performance is therefore anticipated
453 subject to variation in structural parameters. In this case variation in wall thickness, as reported
454 by table 2, led to an overly compliant structure, meaning the structure was unable to sufficiently
455 mitigate the impact. The negative performance was compounded over successive impacts,
456 yielding a larger spike in acceleration as an increasing proportion of kinetic energy was
457 mitigated within the densification region. Conversely, the wall thickness for the PLA_{opt}
458 configuration exceeded the design value. Over successive impacts, the performance, however,
459 improved. In both cases, repeat impact loading causes the base material to transition into its
460 relaxed state due to cyclic stress softening [31] known as the Mullins effect . In the polymer's
461 relaxed state, the resultant stress is lower for the same strain compared to the initial response.
462 Considering the experimental PLA_{opt} results, the initial response was overly stiff, deforming at
463 high stress and did not densify. The consequence of this was a larger resultant acceleration than
464 that anticipated in the computational result. During the subsequent impacts, the structure
465 deformed at lower stress due to the relaxation of the base material. The structure then proceeded
466 to deform at a lower stress, yielding a reduced resultant acceleration whilst deforming further
467 as characterised by nearly reaching densification. These results align with previous studies and
468 indicates that there is opportunity for helmets to be pre-stressed (cycled / conditioned) to
469 achieve repeatable, consistent behaviour [38]. This structure would be more long living than
470 polymeric foams such as EPS, which tend to either plastically deform or demonstrate
471 permanent set [25]. Consequently, this could benefit the user by reducing the risk of
472 unknowingly wearing a helmet that is already damaged, from an innocuous drop or following
473 an impact.

474

475 The finite element model used in this study consisted of a 2 x 2 array with a cell width of
476 12.5mm, representing a 4 x 4 array with a total contact area of 50 x 50mm equivalent to

477 2500mm². Contact area, however, is likely to change on a user-by-user basis as a function of
478 head and helmet radii [47]. Previous investigations adopted a similar contact area values when
479 investigating impact mitigation materials for helmet applications [32] although there seems to
480 be little justification for this design choice. Moreover, other examples exist where a value as
481 high as 6400 mm² has been used for similar impact conditions [48]. Increasing contact area for
482 the same resistive force will yield a reduction in local stress exposed to the user. Therefore,
483 selecting an appropriate contact area is paramount for future investigations. Analytical
484 expression exists for the anticipated contact area based on helmet and head radius, and liner
485 crush [49]. Considering general values for a size J headform, and a nominal liner crush of
486 0.5mm/mm for a 25mm liner, the contact area is in fact 10,000 mm². This exceeds the value
487 used in this study, as well as previous studies, suggesting that an additional performance gain
488 can be achieved through greater consideration of the anticipated contact area.

489

490 Whilst the optimised configurations satisfied the design standard performance threshold, the
491 samples exceeded the typical mass of polymeric foam commonly used in helmet liners, 5g
492 (80g/L [50]), by 10 - 20g. Adopting a stiffer base material with similar elasticity would allow
493 use of thinner walls whilst enabling weight reduction and retaining performance. This could be
494 achieved through different grades of powder [51], or inclusion of additives, such as functional
495 reinforcement [52] and infiltration of resin [53] to improve the base material mechanical
496 properties. Consequently, there is potential for further improvements in performance through
497 adoption of additives within laser sintering to fabricate the pre-buckled honeycomb structure
498 for multi-use helmet liner development.

499

500 The current optimisation process is guided by the design standards that prescribe a vertical
501 impact and a minimum acceptable level of protection.-This, however, is contrary to the fact
502 that the most commonly occurring helmet impact occur at an angle [54]. The forces that arise,
503 therefore, have components of compression and shear [55], [56], [57] which ultimately leads
504 to a rotational velocity and acceleration. It is widely accepted that the human head is susceptible
505 to rotational kinematics [58] and that these loading regimes are more closely linked to traumatic
506 brain injury [59], [60]. Consequently, future optimisation should include angled impact
507 conditions as well as consider other head impact variables such as velocity, location, and
508 curvature of the head.

509

510 **5. Conclusion**

511 In this study, an effective combined numerical framework was reported for optimisation of a
512 parametrically defined honeycomb-type structure, subject to the boundary conditions of a
513 common helmet design standard. Numerical optimisation was realised through use of an
514 algorithm derived from a radial basis function based on finite element analysis, to form a
515 surrogate model of the impact performance relative to the honeycomb's structural parameters.
516 Samples were fabricated using laser sintering of a thermoplastic polyurethane powder ,
517 subjected to experimental impact conditions to validate the outcome of the numerical analysis,
518 then to successive impacts to explore multi-impact behaviour and performance degradation.

519

520 Numerical optimisation revealed the influence of objective function on the impact behaviour
521 for this class of additively manufactured elastomeric honeycomb. For the limits prescribed in
522 the analysis, optimising for peak linear acceleration resulted in a structure that mitigates the
523 kinetic energy of the impact at a stress which facilitates avoidance of the densification region.
524 In contrast, optimising for head injury criterion results in a structure which yields at a relatively
525 lower yield stress and resultant acceleration, however, densifies thus resulting in a higher peak
526 linear acceleration but for a small duration. Fabrication and experimental testing of the samples
527 provided further insights regarding the impact performance. Both structures satisfied their
528 respective objective function when subjected to experimental testing, therefore providing
529 validity for the numerical procedure and its adoption in future studies. Over repeat impacts,
530 PLA optimised structures reported improved performance and stabilised after the third impact.
531 performance was observed over multiple impacts, stabilizing after the third impact. In contrast,
532 HIC optimised structures reported degrading performance over successive impacts. The
533 culmination of this study is a numerical design pathway for exploring new materials and
534 structures for head impact protection.

535

536 **6. Acknowledgements**

537 R. Adams' PhD is part-sponsored by COMFG Ltd. (Charles Owen, Royal Works, Croesfoel
538 Ind. Park, Wrexham, LL14 4BJ, UK). S. Townsend was supported by a grant from the Head
539 Health Tech V competition.

540

541

542 **7. Appendix**

543 Table A1: Hyperelastic material model coefficients (Ogden N5). Adopted from [37].

N	μ	α	D
1	903.01	3.72	0
2	-723.56	5.24	0
3	264.03	6.19	0
4	-669.43	2.26	0
5	236.66	1.42	0

544

545 Table A2: Linear viscoelastic material model coefficients (Prony series). Adopted from [37].

N	G	K	τ
1	0.16	0	1.35E-03
2	0.13	0	7.13E-02
3	8.98E-02	0	0.92
4	7.29E-02	0	6.27
5	8.04E-02	0	49.41

546

547 **8. References**

- 548 [1] D. S. McNally and S. Whitehead, "A computational simulation study of the influence
549 of helmet wearing on head injury risk in adult cyclists," *Accid. Anal. Prev.*, vol. 60, pp.
550 15–23, Nov. 2013.
- 551 [2] N. Dodds *et al.*, "Evaluating the impact of cycle helmet use on severe traumatic brain
552 injury and death in a national cohort of over 11000 pedal cyclists: A retrospective
553 study from the NHS England Trauma Audit and Research Network dataset," *BMJ*
554 *Open*, vol. 9, no. 9, p. e027845, Sep. 2019.
- 555 [3] A. E. Forbes, J. Schutzer-Weissmann, D. A. Menassa, and M. H. Wilson, "Head injury
556 patterns in helmeted and non-helmeted cyclists admitted to a London Major Trauma
557 Centre with serious head injury," *PLoS One*, vol. 12, no. 9, p. e0185367, Sep. 2017.
- 558 [4] M. Bottlang, A. Rouhier, S. Tsai, J. Gregoire, and S. M. Madey, "Impact Performance
559 Comparison of Advanced Bicycle Helmets with Dedicated Rotation-Damping
560 Systems," *Ann. Biomed. Eng.*, vol. 48, no. 1, pp. 68–78, Jan. 2020.
- 561 [5] A. F, D. K, Z. K, S. H, and G. M, "A New Assessment of Bicycle Helmets: The Brain
562 Injury Mitigation Effects of New Technologies in Oblique Impacts," *Ann. Biomed.*

- 563 *Eng.*, 2021.
- 564 [6] “Helmets: a road safety manual for decision-makers and practitioners,” Geneva, 2006.
- 565 [7] D. C. Thompson, F. P. Rivara, and R. Thompson, “Helmets for preventing head and
566 facial injuries in bicyclists,” *Nurs. Times*, vol. 97, no. 43, p. 41, 2001.
- 567 [8] N. Melo, R. J. Berg, and K. Inaba, “Injuries sustained by bicyclists,” *Trauma*, vol. 16,
568 no. 3, pp. 183–188, May 2014.
- 569 [9] A. S. McIntosh *et al.*, “Sports helmets now and in the future,” *Br. J. Sports Med.*, vol.
570 45, no. 16, pp. 1258–1265, Dec. 2011.
- 571 [10] S. P. Soe, P. Martin, M. Jones, M. Robinson, and P. Theobald, “Feasibility of
572 optimising bicycle helmet design safety through the use of additive manufactured TPE
573 cellular structures,” *Int. J. Adv. Manuf. Technol.*, vol. 79, no. 9–12, pp. 1975–1982,
574 Mar. 2015.
- 575 [11] S. F. Khosroshahi, S. A. Tsampas, and U. Galvanetto, “Feasibility study on the use of
576 a hierarchical lattice architecture for helmet liners,” *Mater. Today Commun.*, vol. 14,
577 pp. 312–323, Mar. 2018.
- 578 [12] S. F. Khosroshahi, H. Duckworth, U. Galvanetto, and M. Ghajari, “The effects of
579 topology and relative density of lattice liners on traumatic brain injury mitigation,” *J.*
580 *Biomech.*, vol. 97, p. 109376, Dec. 2019.
- 581 [13] E. C. Clough, T. A. Plaisted, Z. C. Eckel, K. Cante, J. M. Hundley, and T. A.
582 Schaedler, “Elastomeric Microlattice Impact Attenuators,” *Matter*, vol. 1, no. 6, pp.
583 1519–1531, Dec. 2019.
- 584 [14] L. J. Gibson and M. F. Ashby, *Cellular solids: Structure and properties, second*
585 *edition*. Cambridge University Press, 2014.
- 586 [15] T. Thomas and G. Tiwari, “Crushing behavior of honeycomb structure: a review,” *Int.*
587 *J. Crashworthiness*, 2019.
- 588 [16] Z. Wang, “Recent advances in novel metallic honeycomb structure,” *Composites Part*
589 *B: Engineering*, vol. 166. Elsevier Ltd, pp. 731–741, 01-Jun-2019.
- 590 [17] F. Kholoosi and S. A. Galehdari, “Design, optimisation and analysis of a helmet made
591 with graded honeycomb structure under impact load,” *Int. J. Crashworthiness*, vol. 24,
592 no. 6, pp. 645–655, Nov. 2019.
- 593 [18] N. S. Ha and G. Lu, “Thin-walled corrugated structures: A review of crashworthiness
594 designs and energy absorption characteristics,” *Thin-Walled Struct.*, vol. 157, p.
595 106995, Dec. 2020.
- 596 [19] S. Li, Z. Xiao, Y. Zhang, and Q. M. Li, “Impact analysis of a honeycomb-filled

- 597 motorcycle helmet based on coupled head-helmet modelling,” *Int. J. Mech. Sci.*, vol.
598 199, p. 106406, Jun. 2021.
- 599 [20] G. D. Caserta, L. Iannucci, and U. Galvanetto, “Shock absorption performance of a
600 motorbike helmet with honeycomb reinforced liner,” *Compos. Struct.*, vol. 93, no. 11,
601 pp. 2748–2759, 2011.
- 602 [21] E. Bliven *et al.*, “Evaluation of a novel bicycle helmet concept in oblique impact
603 testing,” *Accid. Anal. Prev.*, vol. 124, pp. 58–65, Mar. 2019.
- 604 [22] M. L. Bland, D. S. Zuby, B. C. Mueller, and S. Rowson, “Differences in the protective
605 capabilities of bicycle helmets in real-world and standard-specified impact scenarios,”
606 *Traffic Inj. Prev.*, 2018.
- 607 [23] K. Hansen *et al.*, “Angular Impact Mitigation system for bicycle helmets to reduce
608 head acceleration and risk of traumatic brain injury,” *Accid. Anal. Prev.*, vol. 59, pp.
609 109–117, Oct. 2013.
- 610 [24] S. K. Bhudolia, G. Gohel, and K. F. Leong, “Enhanced energy absorption
611 characteristics of novel integrated hybrid honeycomb/polystyrene foam,” *J. Cell.*
612 *Plast.*, Oct. 2020.
- 613 [25] C. G. Mattacola, C. Quintana, J. Crots, K. I. Tumlin, and S. Bonin, “Repeated impacts
614 diminish the impact performance of equestrian helmets,” *J. Sport Rehabil.*, vol. 28, no.
615 4, pp. 368–372, May 2019.
- 616 [26] R. J. Bromell and D. C. Geddis, “Child cyclists: A study of factors affecting their
617 safety,” *J. Paediatr. Child Health*, vol. 53, no. 2, pp. 145–148, Feb. 2017.
- 618 [27] B. Hanna *et al.*, “Auxetic Metamaterial Optimisation for Head Impact Mitigation in
619 American Football,” *Int. J. Impact Eng.*, p. 103991, Jul. 2021.
- 620 [28] C. Yang, H. D. Vora, and Y. Chang, “Behavior of auxetic structures under
621 compression and impact forces,” 2018.
- 622 [29] S. R. G. Bates, I. R. Farrow, and R. S. Trask, “3D printed polyurethane honeycombs
623 for repeated tailored energy absorption,” *Mater. Des.*, vol. 112, pp. 172–183, Dec.
624 2016.
- 625 [30] S. R. G. Bates, I. R. Farrow, and R. S. Trask, “Compressive behaviour of 3D printed
626 thermoplastic polyurethane honeycombs with graded densities,” *Mater. Des.*, vol. 162,
627 pp. 130–142, 2019.
- 628 [31] R. Adams, S. Townsend, S. Soe, and P. Theobald, “Mechanical behaviour of
629 additively manufactured elastomeric pre-buckled honeycombs under out-of-plane
630 quasi-static and impact loading (Under Review By Journal),” *Mater. Des.*, vol. TBC.

- 631 [32] S. Townsend, R. Adams, M. Robinson, B. Hanna, and P. Theobald, “3D printed
632 origami honeycombs with tailored out-of-plane energy absorption behavior,” *Mater.*
633 *Des.*, vol. 195, p. 108930, 2020.
- 634 [33] V. Caccese, J. R. Ferguson, and M. A. Edgecomb, “Optimal design of honeycomb
635 material used to mitigate head impact,” *Compos. Struct.*, vol. 100, pp. 404–412, Jun.
636 2013.
- 637 [34] T. Whyte *et al.*, “A Review of Impact Testing Methods for Headgear in Sports:
638 Considerations for Improved Prevention of Head Injury Through Research and
639 Standards,” *J. Biomech. Eng.*, vol. 141, pp. 70803–70804, 2019.
- 640 [35] “BS EN 1078: Helmets for pedal cyclists and for users of skateboards and roller
641 skates,” London, 2012.
- 642 [36] “EN 960: Headforms for use in the testing of protective helmets,” 2006.
- 643 [37] R. Adams *et al.*, “A novel pathway for efficient characterisation of additively
644 manufactured thermoplastic elastomers,” *Mater. Des.*, vol. 180, p. 107917, 2019.
- 645 [38] M. Robinson *et al.*, “Mechanical characterisation of additively manufactured
646 elastomeric structures for variable strain rate applications,” *Addit. Manuf.*, vol. 27, pp.
647 398–407, May 2019.
- 648 [39] F. F. Abayazid and M. Ghajari, “Material characterisation of additively manufactured
649 elastomers at different strain rates and build orientations,” *Addit. Manuf.*, vol. 33, p.
650 101160, May 2020.
- 651 [40] J. Hutchinson, M. J. Kaiser, and H. M. Lankarani, “The Head Injury Criterion (HIC)
652 functional,” *Appl. Math. Comput.*, vol. 96, no. 1, pp. 1–16, Oct. 1998.
- 653 [41] H.-M. Gutmann, “A Radial Basis Function Method for Global Optimization,” *J. Glob.*
654 *Optim. 2001 193*, vol. 19, no. 3, pp. 201–227, Mar. 2001.
- 655 [42] E. Acar, “Simultaneous optimization of shape parameters and weight factors in
656 ensemble of radial basis functions,” *Struct. Multidiscip. Optim.*, vol. 49, no. 6, pp.
657 969–978, Dec. 2014.
- 658 [43] L. Verbelen *et al.*, “Analysis of the material properties involved in laser sintering of
659 thermoplastic polyurethane,” *Addit. Manuf.*, vol. 15, pp. 12–19, May 2017.
- 660 [44] N. J. Mills, *Polymer Foams Handbook: Engineering and Biomechanics Applications*
661 *and Design Guide*. 2007.
- 662 [45] F. Shen, W. Zhu, K. Zhou, and L. L. Ke, “Modeling the temperature, crystallization,
663 and residual stress for selective laser sintering of polymeric powder,” *Acta Mech.*, vol.
664 232, no. 9, pp. 3635–3653, 2021.

- 665 [46] J. Versace, "A review of the Severity Index," in *SAE Technical Papers*, 1971.
- 666 [47] H. Mustafa, T. Y. Pang, T. Ellena, and S. H. Nasir, "Impact attenuation of user-centred
667 bicycle helmet design with different foam densities," in *Journal of Physics:
668 Conference Series*, 2019, vol. 1150, no. 1.
- 669 [48] Y. Mosleh, J. Vander Sloten, B. Depreitere, and J. Ivens, "Novel Composite Foam
670 Concept for Head Protection in Oblique Impacts," *Adv. Eng. Mater.*, vol. 19, no. 10, p.
671 1700059, Oct. 2017.
- 672 [49] F. M. Shuaeib, A. M. S. Hamouda, M. M. Hamdan, R. S. Radin Umar, and M. S. J.
673 Hashmi, "Motorcycle helmet: Part II. Materials and design issues," *J. Mater. Process.
674 Technol.*, vol. 123, no. 3, pp. 422–431, May 2002.
- 675 [50] N. J. Mills and A. Gilchrist, "Bicycle helmet design," *Proc. Inst. Mech. Eng. Part L J.
676 Mater. Des. Appl.*, vol. 220, no. 4, pp. 167–180, 2006.
- 677 [51] L. Verbelen *et al.*, "Analysis of the material properties involved in laser sintering of
678 thermoplastic polyurethane," *Addit. Manuf.*, vol. 15, pp. 12–19, May 2017.
- 679 [52] R. D. Goodridge, C. J. Tuck, and R. J. M. Hague, "Laser sintering of polyamides and
680 other polymers," *Prog. Mater. Sci.*, vol. 57, no. 2, pp. 229–267, Feb. 2012.
- 681 [53] Y. Wen *et al.*, "Enhancement of mechanical properties of metamaterial absorber based
682 on selective laser sintering and infiltration techniques," *Compos. Commun.*, vol. 21, p.
683 100373, Oct. 2020.
- 684 [54] N. Bourdet, C. Deck, R. P. Carreira, and R. Willinger, "Head impact conditions in the
685 case of cyclist falls:," <http://dx.doi.org/10.1177/1754337112442326>, vol. 226, no. 3–4,
686 pp. 282–289, Apr. 2012.
- 687 [55] C. Ling, J. Ivens, P. Cardiff, and M. D. Gilchrist, "Deformation response of EPS foam
688 under combined compression-shear loading. Part I: Experimental design and quasi-
689 static tests," *Int. J. Mech. Sci.*, vol. 144, pp. 480–489, Aug. 2018.
- 690 [56] N. Bailly, Y. Petit, J.-M. Desrosier, O. Laperriere, S. Langlois, and E. Wagnac, "Strain
691 Rate Dependent Behavior of Vinyl Nitrile Helmet Foam in Compression and
692 Combined Compression and Shear," *Appl. Sci. 2020, Vol. 10, Page 8286*, vol. 10, no.
693 22, p. 8286, Nov. 2020.
- 694 [57] C. Ling, J. Ivens, P. Cardiff, and M. D. Gilchrist, "Deformation response of EPS foam
695 under combined compression-shear loading. Part II: High strain rate dynamic tests,"
696 *Int. J. Mech. Sci.*, vol. 145, pp. 9–23, Sep. 2018.
- 697 [58] A. H. S. Holbourn, "Mechanics of Head Injuries," *Lancet*, vol. 242, no. 6267, pp. 438–
698 441, Oct. 1943.

- 699 [59] G. TA, "Mechanisms of brain injury.," *J. Emerg. Med.*, vol. 11 Suppl 1, no. SUPPL. 1,
700 pp. 5–11, Jan. 1993.
- 701 [60] A. I. King, J. S. Ruan, C. Zhou, W. N. Hardy, and T. B. Khalil, "Recent Advances in
702 Biomechanics of Brain Injury Research: A Review," <https://home.liebertpub.com/neu>,
703 vol. 12, no. 4, pp. 651–658, Jan. 2009.
- 704